

**Highlights:**

- Progress in the rational design of cationic lipids
- Outlook on the influence of cationic lipid domains on nucleic acids complexation and delivery
- Outlook on the influence of cationic lipid composition on its ultimate geometry and supramolecular structures of lipoplexes

1 **Review Article**

2

3 **Title:**

4 Cationic lipids for gene delivery: many players, one goal

5

6 **Authors' List**

7 Federica Ponti<sup>1,2</sup>, Matilde Campolungo<sup>1</sup>, Clara Melchiori<sup>1</sup>, Nina Bono<sup>1\*</sup> and Gabriele  
8 Candiani<sup>1\*</sup>

9 <sup>1</sup> GenT Lab, Dept. Chemistry, Materials and Chemical Engineering "G. Natta", Politecnico di  
10 Milano, 20131 Milan, Italy

11 <sup>2</sup> Laboratory for Biomaterials and Bioengineering, Canada Research Chair I in Biomaterials  
12 and Bioengineering for the Innovation in Surgery, Dept. Min-Met-Materials Engineering,  
13 Research Center of CHU de Quebec, Division of Regenerative Medicine, Laval University,  
14 Quebec City, QC, Canada

15

16 \* Corresponding authors:

17 Nina Bono and Gabriele Candiani

18 GenT Lab, Dept. Chemistry, Materials and Chemical Engineering "G. Natta", Politecnico di  
19 Milano, 20131 Milan, Italy

20 Via L. Mancinelli, 7 – 20131 Milan (Italy)

21 e-mail: [nina.bono@polimi.it](mailto:nina.bono@polimi.it); [gabriele.candiani@polimi.it](mailto:gabriele.candiani@polimi.it)

22 tel.: +39-02-2399-4741 (NB); +39-02-2399-3181 (GC)

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1 **Abstract**

2 Lipid-based carriers represent the most widely used alternative to viral vectors for gene  
3 expression and gene silencing purposes. This class of non-viral vectors is particularly  
4 attractive for their ease of synthesis and chemical modifications to endow them with desirable  
5 properties. Despite combinatorial approaches have led to the generation of a large number of  
6 cationic lipids displaying different supramolecular structures and improved behavior, additional  
7 efforts are needed towards the development of more and more effective cationic lipids for  
8 transfection purposes.

9 With this review, we seek to highlight the great progress made in the design of each and every  
10 constituent domain of cationic lipids, that is, the chemical structure of the headgroup, linker  
11 and hydrophobic moieties, and on the specific effect on the assembly with nucleic acids. Since  
12 the complexity of such systems is known to affect their performances, the role of formulation,  
13 stability and phase behavior on the transfection efficiency of such assemblies will be  
14 thoroughly discussed. Our objective is to provide a conceptual framework for the development  
15 of ever more performing lipid gene delivery vectors.

16

17 **Highlights:**

- 18 • Progress in the rational design of cationic lipids
- 19 • Outlook on the influence of cationic lipid domains on nucleic acids complexation and  
20 delivery
- 21 • Outlook on the influence of cationic lipid composition on its ultimate geometry and  
22 supramolecular structures of lipoplexes

23

24 **Abbreviations:**

25 NAs, nucleic acids; DNA, deoxyribonucleic acid; RNA, ribonucleic acid; ASO, anti-sense  
26 oligonucleotide; CMC, critical micellar concentration; SAR, structure-activity relationship;  
27 DOTMA, 2-di-O-octadecenyl-3-trimethylammonium propane; DOTAP, 1,2-dioleoyloxy-3-  
28 [trimethylammonium]-propane; DOPE, 1,2-Dioleoyl-sn-glycero-3-phosphoethanolamine;  
29 Chol, cholesterol; GSH glutathione; DSC, differential scanning calorimetry; SAXS, small angle  
30 X-ray scattering; CR, charge ratio; CME, clathrin-mediated endocytosis; CvME, caveolae-  
31 mediated endocytosis

32

33 **Keywords:** non-viral gene delivery; cationic lipids; lipoplexes; transfection; structure-activity  
34 relationship; complexation

35

## 1 1. Introduction

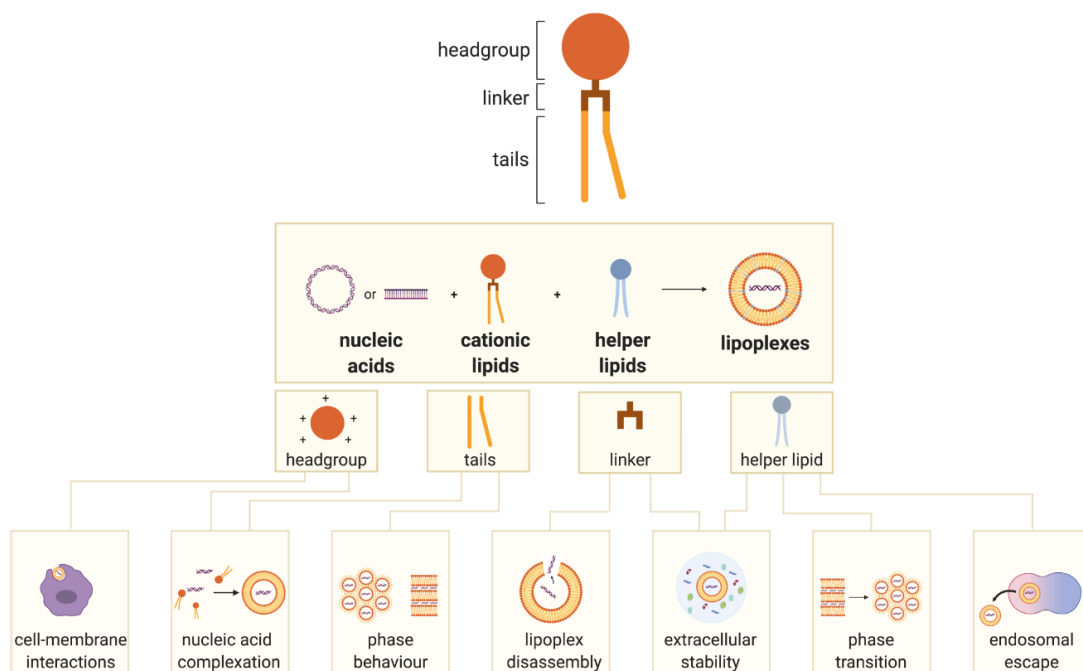
2 Over the last few decades, the delivery of nucleic acids (NAs) as molecular therapeutics  
3 has gathered much attention. The concept of introducing exogenous NAs into host cells (i.e.,  
4 transfection) **has** been extensively exploited to tune the expression of specific proteins in  
5 target cells for manifold purposes (Buck et al., 2019). For instance, gene delivery means are  
6 nowadays essential for the exploitation of some therapeutics, such as those relying on the use  
7 of the CRISPR-Cas9 gene editing technology (Ahmad and Amiji, 2018) **or gene vaccines**  
8 **(Jackson et al., 2020; Walsh et al., 2020).**

9 **As a rule of thumb,** gene delivery techniques and technologies allow the delivery of NAs,  
10 including plasmid DNA (pDNA) **and** messenger RNA (mRNA), **as well as** short regulatory  
11 RNAs, such as small interfering RNA (siRNA), micro RNA (miRNA) and short hairpin RNA  
12 (shRNA), and anti-sense oligonucleotides (ASOs) (for additional information please refer to  
13 (Duvall et al., 2013; Giacca, 2010; **Ginn et al., 2018**)). Despite the delivery of naked NAs  
14 represents the safest way to transfect cells, such procedure is rather ineffective because they  
15 are inherently anionic at physiological pH such that they cannot passively enter cells. In  
16 addition, in this form they are very prone to nucleases-mediated degradation (Al-Dosari and  
17 Gao, 2009). Hence, the main challenge facing us is to develop more and more effective and  
18 little toxic delivery means that protect and facilitate the transfer of NAs into target cells. The  
19 delivery technologies developed so far belong to one of these classes, namely i) physical  
20 methods (Mellott et al., 2013) and ii) vectors (Bono et al., 2020; Lukashev and Zamyatnin,  
21 2016).

22 Physical methods rely on the application of exogenous physical stimuli that allow NAs to  
23 cross the cell membrane and reach the cytosol (for instance inducing a transient disruption of  
24 the plasma membrane) and/or the nucleus (e.g., by means of microneedles) without the use  
25 of any carrier (Wells, 2004). Although such methods have been found somewhat effective  
26 (Mehier-Humbert and Guy, 2005), major drawbacks **relying on their inherent toxicity and the**  
27 ***in vivo* translatability** have limited their widespread application as well.

28 Conversely, vectors are vehicles able to shield the NAs into particle-like assemblies and  
29 ferry them into cells (Patil et al., 2019; Pezzoli et al., 2012; Pezzoli and Candiani, 2013).  
30 Vectors are broadly categorized as viral and non-viral. Viral vectors, that is, engineered viruses  
31 in which a gene cassette encoding desirable traits is in place of the viral genome, are at  
32 present the most effective NAs vehicles, because they take advantage of the inherent ability  
33 of wild-type viruses to productively infect cells (for additional information on viral vectors  
34 please refer to (Finer and Glorioso, 2017; Lukashev and Zamyatnin, 2016; Mancheño-Corvo  
35 and Martín-Duque, 2006)). However, some drawbacks related to viral tropism (i.e., the  
36 specificity of a virus for infecting a particular cell type), inflammatory potential, rather limited  
37 packing capacity and poor safety profile, have prompted the search for the other class of gene  
38 carriers (Jin et al., 2014). Cationic lipids and polymers have gained increasing attention and  
39 have thus become the most studied and used vectors (Bono et al., 2020). These carriers  
40 spontaneously self-assemble with anionic NAs through electrostatic interactions to form nano-  
41 or microparticles, namely lipoplexes and polyplexes, respectively, which provide NAs  
42 protection against nuclease degradation and drive the genetic cargo into cells. The main  
43 reasons why non-viral vectors are really on the rise rely on the greater packing capacity as  
44 compared to viral counterparts and, even more exciting, on the ease of tailoring most of their  
45 specific features (e.g., size, charge, molecular structure) in order to tune and improve their  
46 gene transfer behavior (Hill et al., 2016).

1 With this in mind, this review takes stock of cationic lipids for non-viral gene delivery. They  
 2 are positively charged amphiphiles with a molecular architecture somewhat similar to that of  
 3 natural lipids, with the major difference being the cationic headgroup (Martin et al., 2005;  
 4 Niculescu-duvaz et al., 2003; Rao, 2010). When exposed to an aqueous environment and  
 5 above a certain critical micellar concentration (CMC), they spontaneously arrange in intriguing  
 6 three-dimensional (3D) assemblies, namely lamellar, micellar, or inverted hexagonal phases,  
 7 depending on the composition and structure of the lipid itself (Wasungu and Hoekstra, 2006).  
 8 Since the seminal work of Felgner and colleagues in late 80s about the use of cationic lipids  
 9 for lipofection (i.e., the transfection of cells using lipid-based transfectants) (Felgner et al.,  
 10 1987), much has been done in the way of developing a number of lipids and lipid formulations  
 11 for the delivery of a wide range of NAs of different molecular weight ( $M_w$ ), including large  
 12 pDNAs ( $M_w < 10$  kbase pairs) (Buck et al., 2019; Hirko et al., 2005) and messenger RNAs  
 13 (mRNAs) ( $M_w < 10$  kbases) (Guan and Rosenecker, 2017; Hajj and Whitehead, 2017), and  
 14 short sequences such as siRNAs ( $M_w \approx 15-30$  mers) (Rietwyk and Peer, 2017; Shim et al.,  
 15 2013; Zhang et al., 2007). Broadly speaking, cationic lipids consist of three different domains,  
 16 that is, a *cationic headgroup*, covalently bound through a *linker* to a *hydrophobic tail* (Martin  
 17 et al., 2005) (**Figure 1**). Interestingly, each of them plays a pivotal role in the delivery process  
 18 of NAs, so that each and every of these moieties can be suitably tailored to fine-tune the  
 19 behavior of the resulting complexes. It is worthy of note that, even if the effect of each domain  
 20 on the overall lipoplex behavior has been extensively but separately studied (Zhi et al., 2018,  
 21 2013, 2010), the joint effects of the combination of the three have seldom been faithfully  
 22 depicted, so that the reader may find it difficult to see the forest and the trees. Nonetheless,  
 23 due to the inherent complexity of the cells-to-lipoplexes interplay and *vice versa*, a  
 24 comprehensive big picture depicting reciprocal interactions between such living and non-living  
 25 matter is far from being drawn up (Ewert et al., 2010). In this context, the thorough  
 26 understanding and knowledge of the uptake mechanisms of transfectant/NAs particles and  
 27 their intracellular trafficking would lead to the rational design of more effective non-viral lipid-  
 28 based vectors.



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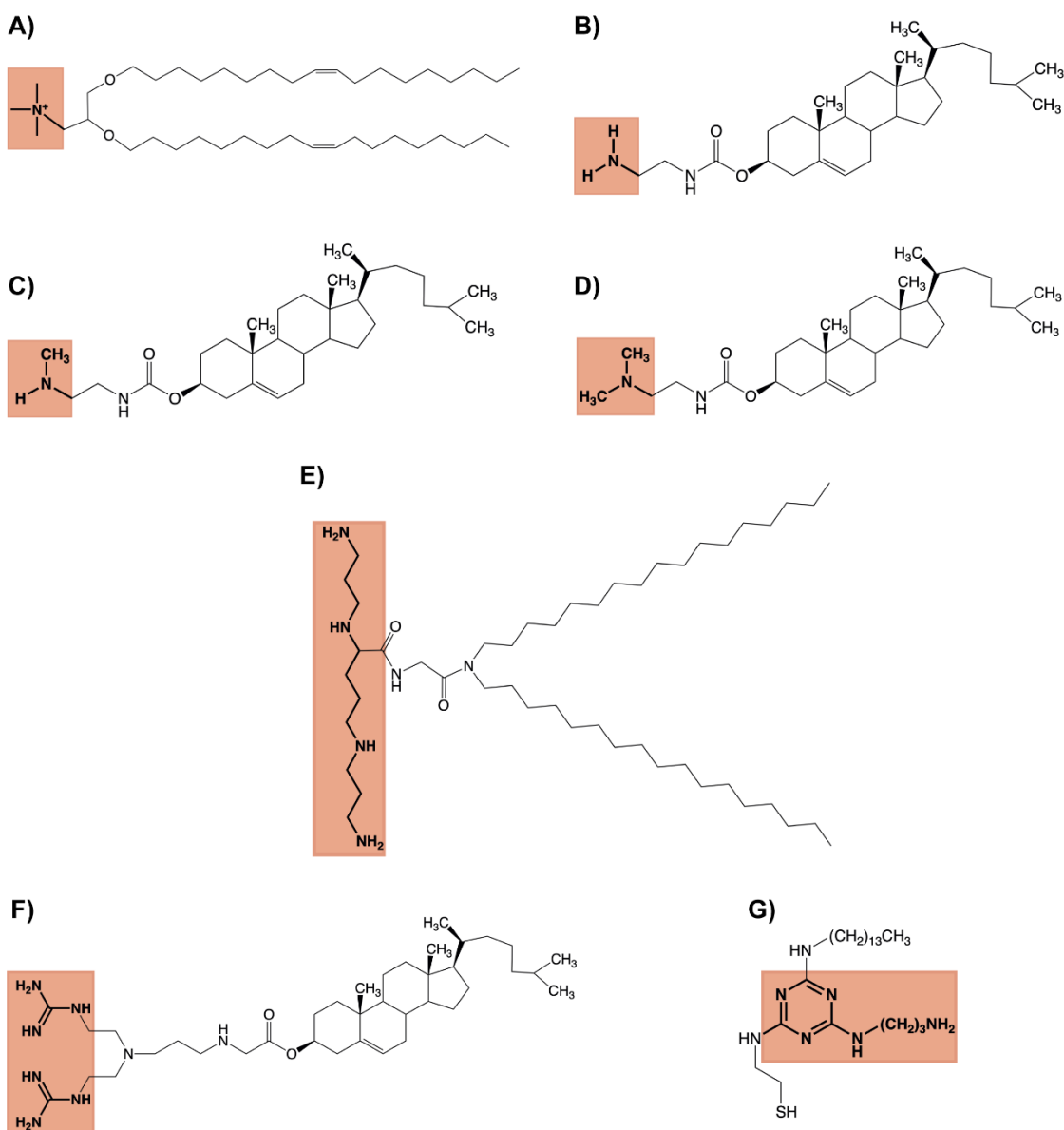
30 **Figure 1** - Schematic representation of the three basic domains of a cationic lipid and their role in the  
 31 complexation and delivery of nucleic acids.

## 2. Molecular structure of cationic lipids

### 2.1. Headgroups

Polar headgroups play a prominent role in binding anionic NAs by means of electrostatic interactions and give rise to complexes, the so-called lipoplexes, made of cationic lipids and NAs. The headgroup features, such as dimension and charge density, are responsible for the lipoplex stability, interaction with the cell membrane and endosomal escape mechanisms, along with NAs compaction, **that is, they** have a huge impact on the **overall performance of lipoplexes** (Zhi et al., 2013).

Depending on the chemical composition, the most prominent classes of polar heads are quaternary ammonium salts, amines (primary, secondary, and tertiary), guanidine, heterocyclic compounds, and a combination thereof (**Figure 2**). More recently, the rational design of novel cationic lipids bearing biomacromolecular headgroups has led to the rise of novel multifunctional carriers with unique delivery properties (Ortiz Mellet et al., 2010).



**Figure 2** - Chemical structure of cationic lipids with different headgroup domains, namely: **A)** DOTMA; **B)** AC-Chol; **C)** MC-Chol; **D)** DC-Chol; **E)** DOGS; **F)** BGTC; **G)** triazine ring-based cationic lipid. Specifically, the headgroup domain of each lipid consists of a **(A)** quaternary ammonium salt, **(B)** primary amine, **(C)** secondary amine, **(D)** tertiary amine, **(E)** polyamine, **(F)** guanidinium group, and a **(G)** melamine group (i.e., a heterocycle). Colored areas highlight polar headgroups.

1 Cationic lipids bearing multivalent headgroups have been proposed as effective  
2 transfectants because able to bind NAs **tightly**, pack and seclude them from the intracellular  
3 environment, so that **they are considered more effective in transfection** than their monovalent  
4 counterparts (Koynova and Tenchov, 2011; Rosenzweig et al., 2001).

5 When in solution, the NAs binding properties of the polar head are strongly dependent on  
6 the pH of the solution, as this influences the protonation of the headgroup itself. The best way  
7 to get insights into the acid-base behavior of a cationic headgroup relies on the acidic  
8 dissociation constant ( $pK_a$ ) of the conjugate acid. Specifically, the higher the  $pK_a$  of the  
9 conjugate acid, the stronger the base. In practice, when cationic lipids are dissolved at  $pH <$   
10  $pK_a$ , their headgroups are protonated, otherwise called cationic, such that the electrostatic  
11 interaction with the NA counterions occurs.

12 Furthermore, the presence of protonatable groups within the headgroup chemical structure  
13 may confer to the amphiphile some buffering activity that can be conveniently exploited to  
14 favor NAs release once in the endosome. For instance, when in the acidic environment of the  
15 endosome ( $pH = 5.5-6$ ), weakly basic sponges display a  $H^+$  buffering activity, thus resulting in  
16 a  $Cl^-$  accumulation within the endosomal compartment, ultimately leading to the swelling of the  
17 vesicle (Budker et al., 1996; Freeman et al., 2013). Since the poor release of the genetic  
18 material from endosomes is believed to be one of the most critical issues hindering the gene  
19 transfer efficiency of lipoplexes, cationic lipids able to exploit such osmotic-driven process,  
20 generally known as proton sponge effect, are widely preferred to strong bases indeed.

21 In this light, the headgroup chemistry is a key aspect in lipid design.

### 22 23 **2.1.1. Quaternary ammonium**

24 Quaternary ammonium ( $NR_4^+$ ) is an organic cation carrying a permanently positively  
25 charged nitrogen atom (N) covalently bound to four organic substituents (R) (**Figure 2**). Due  
26 to their lasting positive net charge at physiological pH, which allows for strong NAs binding  
27 and **high** solubility in aqueous environments (Dizman et al., 2004), quaternary ammonium  
28 headgroups are so far the most frequently used polar heads to build cationic lipids (Sakurai et  
29 al., 2000). The wide range of gene delivery vectors bearing a quaternary ammonium  
30 headgroup includes 1,2-di-O-octadecenyl-3-trimethylammonium propane (DOTMA) (Felgner  
31 et al., 1994) depicted in **Figure 2A**, 1,2-dioleoyloxy-3-[trimethylammonium]-propane (DOTAP)  
32 (Stamatatos et al., 1988), dimethyl-dioctadecyl ammonium bromide (DDAB) (You et al., 1997)  
33 and cetyl-trimethyl ammonium bromide (CTAB) (Pinnaduwege et al., 1989). The former  
34 molecule (**Figure 2A**) was the first quaternary ammonium-bearing lipid to be synthesized and  
35 it is perhaps the most renowned among them all.

36 In order to strengthen the NAs binding behavior of cationic lipids and foster cell membrane  
37 interactions of lipoplexes, some authors devised the hydroxylation of the quaternary  
38 ammonium head of lipid vectors (Berchel et al., 2015; Felgner et al., 1994). Along with those  
39 first evidences, recent works **have** confirmed the improved transfection abilities arising from  
40 such molecular modification with respect to **the quaternary ammonium-bearing precursors**.  
41 For instance, Maiti and colleagues synthesized novel *gemini* surfactants with hydroxyl-  
42 modified quaternary ammonium headgroup, and speculated that the poor hydration of the  
43 head region, that is, its low cross-sectional area, was responsible for the **higher transfection**  
44 **efficiency** the lipids displayed **when compared to the commercially-sourced Lipofectamine**  
45 **2000** (Maiti et al., 2018). In turn, **the decrease in the headgroup hydration resulting from the**  
46 **hydrogen bonding between juxtaposed hydroxyl groups was thought to drive** the formation of  
47 lipoplexes **which were** more prone to phase transition, **such that they eventually fuse** with the  
48 endosome and **release the** NAs (Jones et al., 2013; Zhang et al., 2014). Conversely, along



1 with this destabilizing effect, quaternary ammonium headgroups bearing hydroxyls have  
2 proved to **condense more effectively NAs due to the formation of** hydrogen bonding with NAs,  
3 **such that** the stability of complexes **was improved** (Narang et al., 2005).

### 5 **2.1.2. Primary amines, secondary amines, tertiary amines and polyamines**

6 Amines are derivatives of ammonia classified as primary, secondary, or tertiary whether  
7 one, two or three hydrogen atoms have been replaced by an organic group (**Figure 2B-D**).  
8 Although their acid-base properties are strongly dependent on the number and type of  
9 substituents, amines are generally considered as weak bases. Broadly speaking, secondary  
10 amines (**Figure 2C**) are slightly more basic than primary ones (**Figure 2B**), while tertiary  
11 amines (**Figure 2D**) are less basic than their secondary analogues due to the steric hindrance  
12 of their substituents. The amines basicity mirrors their  $pK_a$  **values**, that is, 10.6, 10.8 and 9.8  
13 for primary, secondary and tertiary amines, respectively, when the substituent is the simple  
14 methyl group (Hall, 1957). Since amine headgroups invariably exhibit a neutral or low cationic  
15 charge at physiological pH, cationic lipids bearing **such kinds** of cationic heads have long half-  
16 life in the body circulation, but also a relatively **poor** NAs binding **ability** (Buck et al., 2019).

17 In an attempt to shed light on the transfection effectiveness of the differently substituted  
18 amine-bearing lipids, Kearns *et al.* synthesized a whole array of cationic cholesterol (Chol)-  
19 based derivatives and found that primary and secondary amines were the most effective  
20 (Kearns et al., 2008). More recently, these results were eventually proven wrong by Lin and  
21 colleagues who showed that tertiary amines featured as the most effective transfectants (Lin  
22 et al., 2019; Liu and Huang, 2010; Semple et al., 2010). Interestingly, because tertiary amines  
23 are weaker bases, it has been hypothesized that they undergo protonation in an acidic  
24 environment, thus conferring lipids with some buffering capacity that is beneficial for  
25 endo/lysosome escape and NAs release within the cell.

26 Polyamines-bearing lipids have emerged as promising transfectants as well (Vijayanathan  
27 et al., 2014). As an example, Cooper and co-workers reported that the newly synthesized  
28 penta-amine  $N^{15}$ -cholesteryloxycarbonyl-3,7,12-triazapentadecane-1,15-diamine (CTAP)  
29 showed a 100-fold increase in transfection efficiency with respect to conventional DC-  
30 Chol/1,2-Dioleoyl-sn-glycero-3-phosphoethanolamine (DOPE) formulation (Cooper et al.,  
31 1998). Because CTAP displays a high charge density, which is dependent on the number of  
32 total amine groups that are fully protonated at physiological pH, the authors speculated that  
33 this would lead to a more effective neutralization, condensation and encapsulation of NAs  
34 (Stewart et al., 2001). Apart from the charge density, Martin *et al.* pointed out the importance  
35 of the headgroup shape on the transfection behavior of polyamine-containing amphiphiles  
36 (Martin et al., 2005). Although branched polyamines are less prone to folding problems, that  
37 is, they display the most stable conformation (Fujiwara et al., 2000; Zhi et al., 2013), they are  
38 generally less efficient than linear compounds. Byk *et al.* compared cationic lipids having  
39 linear, T-shaped, branched and globular headgroups, and reported **that the former showed**  
40 **the highest NAs condensation ability and** transfection efficiency *in vitro* (Byk et al., 1998).  
41 Since the seminal work by Behr's team about the effective linear polyamine-bearing lipid  
42 dioctadecylamidoglycylspermine (DOGS) (**Figure 2E**) (Behr et al., 1989), spermine  
43 headgroup has thus been extensively exploited to design gene delivery vectors (Markov et al.,  
44 2012; Maslov et al., 2012; Niyomtham et al., 2015).

### 45 **2.1.3. Guanidinium headgroup**

46 Guanidine is a strong organic base typically present in arginyl residues involved in DNA-  
47 binding histones (Goebel and Klappo, 2007). It is worthy of note that guanidine ensures strong  
48



1 NAs binding properties (Cotton et al., 1973; Wender et al., 2008) because it exists almost  
2 exclusively in the form of guanidinium cation over a wide range of pH (Xu et al., 2017), with  
3 the charge delocalized over three N that donate lone pair electrons at once (**Figure 2F**).  
4 Guanidinium-bearing carriers are also able to form bidentate hydrogen bonding with the  
5 anionic phospholipids of the cell membrane, which favors the internalization of lipoplexes into  
6 cells (Rothbard et al., 2005). Nonetheless, it has also been reported that guanidinium cation  
7 may negatively impact the effectiveness of gene delivery systems because of the (too) tight  
8 binding with NAs (Bono et al., 2019).

9 From an historical perspective, bis-guanidinium-spermidine-Chol (BGSC) and bis-  
10 guanidinium-tren-Chol (BGTC) (**Figure 2F**) were the first two guanidinium-bearing lipid  
11 transfectants developed (Vigneron et al., 1996). Multivalent forms arising from the conjugation  
12 of the guanidinium group with other cationic moieties, such as pyridinium and amines, have  
13 proven to be more efficient in transfection and less cytotoxic than their monovalent analogues  
14 (Banerjee et al., 2001). As an example, Huang's group synthesized the cationic lipid N,N-  
15 distearyl-N-methyl-N-2[N'-(N<sup>2</sup>-guanidino-L-lysiny)] aminoethyl ammonium chloride (DSGLA)  
16 with a dual head displaying both guanidinium and lysine residues, and showed that it gave  
17 rise to a more effective siRNA binding as compared to the conventional DOTAP (Chen et al.,  
18 2010).

19 One of the most relevant chemical variations of the guanidinium headgroup relies on the  
20 use of amidine substituents, which are organic compounds having the general formula  
21  $RC(NR')NR''_2$ . They are obtained through the replacement of an amine of the guanidine with  
22 a generic R group. Depending on the substituent, the  $pK_a$  may vary from 5 to 12, while  
23 protonation invariably occurs at the imino nitrogen ( $=NR'$ ) (Quek et al., 2013). In this regard,  
24 the patented *gemini* cationic surfactant known as TRX, which bears an amidine in the head  
25 region, did induce a higher percentage of GFP-expressing cells and showed reduced  
26 cytotoxicity than the gold standard Lipofectamine (Koiwai et al., 2005).

#### 27 28 **2.1.4. Heterocyclic headgroups**

29 Pyridine, imidazole and their derivatives have been widely used as cationic heterocyclic  
30 headgroups. Due to their chemical nature, they can act as acids as well as bases, with  
31 imidazole being 100 times more basic than pyridine (Ouellette and Rawn, 2018). Once in  
32 acidic solutions, pyridine and imidazole become protonated and give rise to pyridinium and  
33 imidazolium ions, respectively. Of note, the delocalization of the positive charge throughout  
34 the heterocycle results in a slightly hydrophobic head, which improves the NAs binding-release  
35 behavior (Gaitor et al., 2017) by acting as pH-sensitive moiety. In this regard, relying on such  
36 peculiar feature, Liu *et al.* synthesized a series of cyclen-based cationic lipids bearing an  
37 imidazole headgroup (Liu et al., 2013). Of note, being the  $pK_a$  of this moiety very close to the  
38 endosomal pH, these lipids were able to give rise to the proton sponge effect and to efficiently  
39 transfect cells. Likewise, Berchel and co-workers synthesized  $\alpha$ -amino-phosphonate lipids  
40 displaying two pH-sensitive moieties that were in the protonatable aza-heterocycle (imidazole  
41 or pyridine) (Berchel et al., 2017). Acting as weak bases, such compounds are mostly neutral  
42 at physiological pH, while they become cationic when the pH drops to 6 and even lower. Again,  
43 this resulted in the escape of lipoplexes from the endosomes. It has been recently proposed  
44 that the coupling of different polar heads, such as 1,2,3-triazolium and the conventional  
45 quaternary ammonium headgroup, could give rise to multi-cationic lipids very effective for  
46 gene delivery applications (Gosangi et al., 2017).

47 Besides, among heterocyclic groups, melamine is an organic nitrogenous compound used  
48 in the production of plastics, dyes, fertilizers, fabrics, and it is part of the core structure for a

1 number of drugs. Due to delocalized cationic charge of the s-triazine ring and the easy N-  
2 derivatization of melamine scaffold with different substituents, melamine has also been  
3 profitably used to synthesize cationic lipids for gene delivery (**Figure 2G**) (Candiani et al.,  
4 2007). Likewise, triazacyclononane (TACN)-based lipids have emerged as suitable  
5 transfectants as well. Bearing three N with different  $pK_a$  values, this class of lipids exhibited  
6 delivery abilities **comparable to that of Lipofectamine 2000**. The reason for that relies on the  
7 presence of a N that, at physiological pH, confers some basicity ( $pK_a = 11$ ) to the lipid and  
8 promotes interactions with the DNA, while the other **N-based groups** have  $pK_a \approx 6$  and provide  
9 some buffering ability to lipoplexes once they are in the endosomes (B. Wang et al., 2014;  
10 Zhang et al., 2011).

### 11 **2.1.5. Multifunctional headgroups**

12  
13 Despite the vast majority of cationic lipids have been designed with amine-derived  
14 headgroups, it is generally thought that amino acid-based transfectants can achieve similar or  
15 even higher transfection efficiency and lower cytotoxicity **than commercially sourced lipid**  
16 **transfectants, such as DOTAP and Lipofectamine** (Brito et al., 2009; Zhang et al., 2014; Zhao  
17 et al., 2017). Lysine, arginine, histidine and ornithine have been extensively used as polar  
18 headgroups for the synthesis of lipidic transfectants (Zillner et al., 2012). In this direction, Silva  
19 *et al.* synthesized a series of serine-derived *gemini* surfactants, which have been used alone  
20 or in combination with the helper lipid DOPE to condense pDNA and transfect cells with **some**  
21 success (Silva et al., 2014, 2013). In an attempt to select the most effective amino acid to be  
22 used as the polar head, Obata and co-workers synthesized a series of cationic lipids bearing  
23 lysine, histidine and arginine (Obata et al., 2008). Notably, they showed that histidine-bearing  
24 lipids were not suited to form lipoplexes. This was probably because of the low basicity of the  
25 tertiary amino group of histidine that would account for weaker interactions with NAs than the  
26 primary amino group of lysine or arginine. Other authors reported similar results and provided  
27 some evidence about the **higher** transfection efficiency of lysine- and arginine-bearing cationic  
28 lipids with respect to histidine analogues (Jiang et al., 2016; Sheng et al., 2014). It is worthy  
29 of note that the amino acid lysine is sensitive to pH changes due the presence of two  
30 protonatable amines displaying different  $pK_a$  values. In this light, Walsh and co-workers  
31 reported the synthesis of a series of ionizable lysine-based lipids that exhibited a pH-  
32 dependent protonation behavior (Walsh et al., 2013). At physiological pH such lipids did  
33 proficiently interact with siRNA, but when endocytosed, the lipids became increasingly cationic  
34 and were able to disrupt the endosomes because of the lowering of the pH.

35 Amphiphiles with di- or **tripeptide** headgroups have also been largely **investigated**. For  
36 instance, Zhao and co-workers developed a tri-ornithine peptide-bearing cationic lipid (Zhao  
37 et al., 2017), that was found to be far more effective than the quaternary ammonium-bearing  
38 counterpart in binding and delivering NAs to cells. Of note, such behavior **has** been attributed  
39 to the presence of the tri-ornithine peptide that does undergo protonation at different pH and  
40 facilitate the endosomal escape of lipoplexes.

41 Aminoglycosides-bearing lipids have been found very effective as well. Because  
42 aminoglycosides are a heterogeneous class of polycations with strong NAs binding ability  
43 (Arya et al., 2001; Bono et al., 2019; Ghilardi et al., 2013) and renowned antibacterial  
44 properties (Bera et al., 2010; Fosso et al., 2014; Houghton et al., 2010), they have been  
45 extensively used to give rise to multivalent gene delivery vectors. Just to give some examples,  
46 Lehn's group synthesized and patented very effective lipid derivatives using paromomycin-,  
47 neomycin B, and kanamycin A as headgroups (Mével et al., 2012; Sainlos et al., 2003). More  
48 recently, our group **synthesized** an array of aminoglycosides-modified calixarene lipids **that**

1 showed transfection efficiencies similar or even higher than that of the gold standard branched  
2 polyethylenimine (bPEI), low cytotoxicity and excellent antimicrobial properties against Gram-  
3 negative bacteria (Bono et al., 2018).

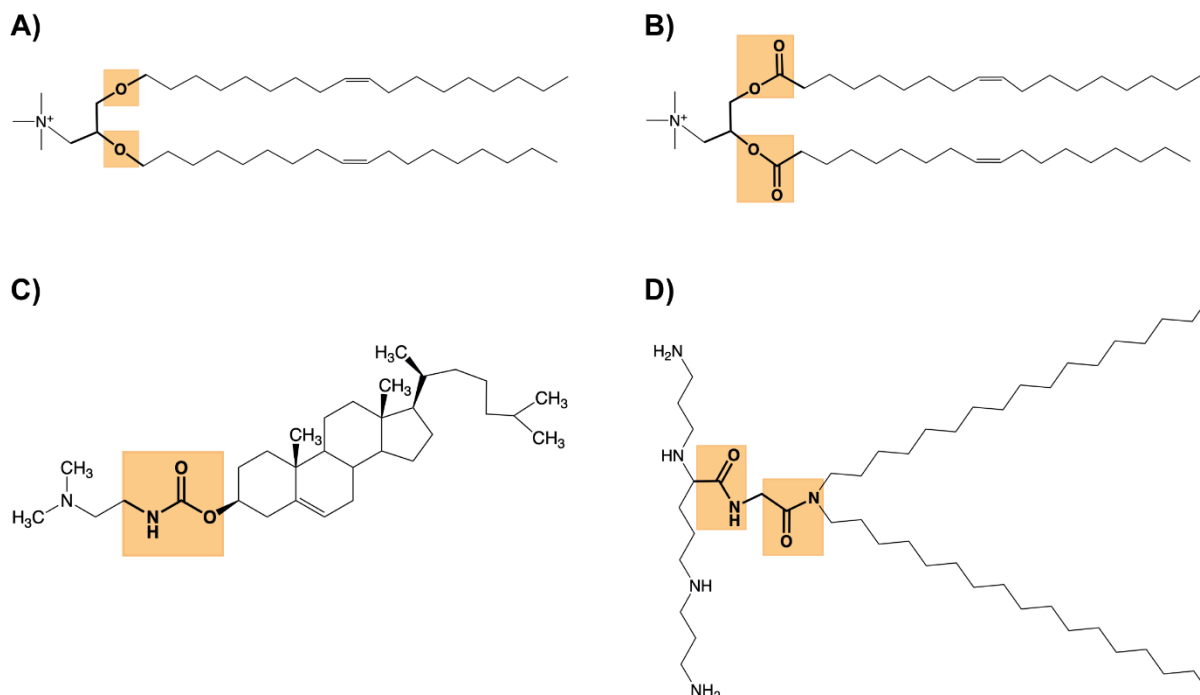
4  
5 Altogether, these findings pointed to ionizable headgroups as the most efficient moieties  
6 in the design of lipids for gene delivery applications. It has been shown that they endow  
7 lipoplexes with endosomal membrane-destabilizing properties that, in turn, are responsible for  
8 the ultimate NAs release in the cytoplasm. As a matter of fact, cationic lipids bearing  
9 protonatable headgroups with  $pK_a < 7$  (e.g., primary and tertiary amines, imidazole and  
10 pyridine) are by far the most effective in transfection.

## 11 2.2. Linkers

12 Being the *trait d'union* between the hydrophilic polar headgroup and the non-polar tail(s),  
13 the linker moiety plays a pivotal role in the behavior of the cationic lipid as a whole, such as  
14 the stability, biodegradability, cytotoxicity, and transfection efficiency (Pezzoli et al., 2012;  
15 Srinivas et al., 2009). In practice, some features of the linker, including the overall charge,  
16 length and steric hindrance, are responsible for the conformational flexibility of the amphiphile.  
17 In other words, the relative orientation of the hydrophobic and cationic moieties affects the  
18 interaction of the lipid with NAs, and in turn, the ultimate gene transfer efficiency (Buck et al.,  
19 2019; Draghici and Ilies, 2015; Fujiwara et al., 2000).

20 Depending on the structure, linkers are grouped into many types, such as ethers,  
21 esters, carbamates, and amides (Figure 3). Of note, some of them have been engineered to  
22 be sensitive to specific stimuli, including pH and redox variations and the action of enzymes,  
23 underpinning behavioral responsiveness to environmental cues (Candiani et al., 2007; Guo et  
24 al., 2014; Nagasaki et al., 2003; Terada et al., 2006).

25 The most significant advances in the linkers design are highlighted and thoroughly  
26 discussed here below.



28  
29 **Figure 3.** Chemical structure of cationic lipids displaying different linkers, namely: A) DOTMA; B)  
30 DOTAP; C) DC-Chol; D) DOGS. Specifically, the headgroup region is connected to the hydrophobic  
31 portion(s) by means of a (A) ether, (B) ester (C) carbamate, and (D) amide. Colored areas highlight  
32 linkers.

### 2.2.1. Ethers

Ether bonds are characterized by the presence of an oxygen (O) atom linked to two alkyl groups (Figure 3A).

It has been shown that the transfection efficiency of the diether-linked cationic lipid, DOTMA (Figure 3A), was 10-fold more effective than that of the diester-containing lipid analogue, DOTAP, when lipoplexes were formed without the addition of helper lipids (Song et al., 1997). By the same token, Ghosh and colleagues reported that ether-containing lipids were much more effective in transfection than the easily-degradable ester- and carbamate-bearing lipids (Ghosh et al., 2000). Despite the superior transfection efficiency of cationic lipids bearing ether linkages, such transfectants do not undergo substantial hydrolysis *in vitro* and *in vivo* (White et al., 1996), which results in some cytotoxicity (Zylberberg et al., 2017). Indeed, because of the high chemical stability of ethers, the cleavage of the C-O bond is uncommon in the absence of specialized reagents or under extreme conditions.

So far, a number of strategies have been envisioned in order to enhance the biodegradability of common ether linkages. Among stimuli-sensitive linkers, acid-labile vinyl-ethers have been widely exploited. The hydrolysis rate of this kind of ethers displays a pseudo first-order dependence on the pH, as the reaction rate accelerates approximately to an order of magnitude for each unit of pH reduction (Gerasimov et al., 1997). In the acidic milieu of lysosomes (pH  $\approx$  4.5), the hydrolysis of the linker occurs through the protonation of the  $\beta$ -carbon of the vinyl-ether (Meyer and Wagner, 2006), which favors some lipid structural changes leading to the release of NAs (Shin et al., 2012, 2003). One practical and most successful example of cationic lipid bearing vinyl-ether groups is represented by O-(2R-1,2-di-O-(1Z,9Z-octadecadienyl)-glycerol)-3-N-(bis-2-aminoethyl)carbamate (BTCA), which has been found to mediate endosomal escape of lipoplexes (Sullivan et al., 2002). Recently, in order to improve the overall biocompatibility of  $\alpha$ -tocopherol-based cationic amphiphiles, Patri's group used ether- $\beta$ -hydroxy-triazole linker that underwent total hydrolysis at the endolysosomal pH. This resulted in the endosomal escape of NAs that, in turn, gave rise to transfection efficiencies similar to that of Lipofectamine 3000 and very low cytotoxicity (Muripiti et al., 2018).

### 2.2.2. Esters

Esters are carboxylic acid derivatives in which the hydroxyl group is replaced by an O-alkyl (alkoxy) moiety (Figure 3B). Acting as hydrogen-bond acceptors, esters are very soluble in water. Of note, ester linkages are prone to both acidic intracellular hydrolysis and endogenous esterase- or lipase-mediated cleavage (Speight, 2017). This kind of linker is therefore easily (bio)degraded. A typical example of ester-bearing cationic lipid is DOTAP in Figure 3B. Given the very promising results in transfections (Fletcher et al., 2006; Leventis and Silviu, 1990), different DOTAP-based lipoplexes entered preclinical and clinical trials (Firouzmand et al., 2013; Lu et al., 2012). On the other hand, the poor chemical stability of the vectors displaying this kind of linkage may even undermine their overall delivery efficacy (Sun et al., 2013). In this regard, a significant reduction in transfection efficiency was reported when alkoxy linker in the 1,2-dilinoleyloxy-3-dimethylaminopropane (DLinDMA) lipid was replaced with an ester linker (Semple et al., 2010).

In an effort to develop pH-sensitive lipoplexes for efficient gene delivery, some scientists have developed novel cationic lipids incorporating ortho-ester linkages. Being one of the most acid-labile linkers, ortho-esters show strong pH-responsiveness, along with great biocompatibility. As an example, Chen *et al.* showed that, at low pH, transfectants bearing ortho-ester linkages were prone to acidic hydrolysis and split apart, such that the interactions

1 between cationic lipids and the DNA became so weak that the genetic cargo was promptly  
2 released into the cytosol (Chen et al., 2013, 2007).

### 3 4 **2.2.3. Carbamates (or urethanes)**

5 Lipoplexes based on cationic lipids incorporating carbamate linkers, also referred to as  
6 urethanes, exhibit improved stability with respect to simple ester counterparts. This results in  
7 excellent transfection properties and poor cytotoxicity (Jin et al., 2014). A typical example of  
8 carbamate-bearing cationic lipid is DC-Chol in **Figure 3C**. Similar to the other linkers, also  
9 carbamates undergo hydrolysis in the endosomal compartment because sensitive to pH shifts.  
10 In addition, Gao and Huang suggested that carbamate linkers are promptly cleaved by  
11 intracellular esterases (Gao and Huang, 1991), so that such kind of linkers are biodegraded  
12 once having entered the cells. All these features have spurred more interest in the design of  
13 cationic lipids with these linkers.

14 Medvedeva and colleagues first reported about the superior transfection behavior of  
15 carbamate-containing lipids as compared to ether, ester analogues and even the gold  
16 standard Lipofectamine. Interestingly, such lipids were found to be less cytotoxic than the  
17 other counterparts (Medvedeva et al., 2009). Similar results were also reported by other  
18 groups dealing with carbamate-containing gemini quaternary ammonium headed lipids (Shi et  
19 al., 2016; Zhao et al., 2014). On the basis of their high transfection efficiency and stability in  
20 extracellular fluids, lipids with a carbamate linker entered gene therapy clinical trials  
21 (McLachlan et al., 2011; Zabner et al., 1997).

### 22 23 **2.2.4. Amides**

24 An amide linkage is a covalent bond occurring in peptides and proteins, with the general  
25 formula sketched in **Figure 3D**. A representative cationic lipid with an amide linkage is DOGS,  
26 in which the linker is used to tether the saturated alkyl chain and the spermine headgroup  
27 (Behr et al., 1989). DOGS-based lipoplexes have been reported to be much more effective in  
28 transfecting cells when compared to DOTAP-based analogues (Paliwal et al., 2015), and this  
29 may be due to their pH-buffering behavior.

30 As a rule of thumb, amide hydrolysis occurring in the acidic environment of the endosome  
31 was found to be very similar to that of ester linkers, that is, the mechanism consisting in the  
32 protonation of the O atom of the amide followed by the attack of water on the carbonyl carbon,  
33 giving rise to a carboxyl acid and an ammonium salt (O'Connor, 1970). Similarly to  
34 carbamates, lipoplexes prepared with pH-sensitive amide-bearing cationic lipids possess  
35 superior stability and reduced cytotoxicity with respect to those containing ester and ether  
36 linkages (Ghosh and Brindisi, 2015). In this light, Vacus and co-workers suggested that the  
37 ability of amide linkers to form intermolecular hydrogen bonding is responsible for the high  
38 melting temperature of the lipids and for the lipoplex stability (Boukhnikachvili et al., 1997).  
39 Such speculations were later confirmed by Gopal *et al.*, who demonstrated that amide-bearing  
40 cationic lipids were much more stable and effective in transfection than ester-tethered  
41 transfectants (Gopal et al., 2011).

42 Besides, it has been shown that the relative orientation of the amide linker with respect to  
43 the cationic headgroup has a striking effect on the transfection behavior of lipoplexes (Srujan  
44 et al., 2011; Vijay Darshan et al., 2014). Specifically, the presence of reverse isomeric amide  
45 groups in the lipid structure showed reduced transfection efficiency with respect to normal-  
46 oriented amide ones (i.e., the amine group of the amide is in close proximity to the polar head),  
47 which, in turn, proved to be as effective as Lipofectamine 2000 in transfecting a wide variety



1 of cells. This was conceivably due the higher rigidity of inverse amide-containing lipids due to  
2 the Coulombic repulsion of the two moieties (Srujan et al., 2011).

### 3 4 **2.2.5. Miscellaneous**

5 Although less common, pH-sensitive, acid-labile linkers with hydrolysis rates similar to  
6 those of carbamates and vinyl-ethers are acetals/ketals (Semple et al., 2010; Zhu et al., 2002)  
7 and hydrazones (Aissaoui et al., 2004).

8 Of note, since ketal bonds display a higher hydrolysis rate at endosomal pH as compared  
9 to neutrality, cationic lipids incorporating this linkage were found to be stable in blood (Zhu et  
10 al., 2002). Likewise, Aissaoui *et al.*, studied the sensitivity of the acylhydrazone function to the  
11 acidic environment of lysosomes and showed that the hydrolysis rate increased under such  
12 conditions (Aissaoui et al., 2004).

13 In addition to acid-labile linkers, redox-sensitive disulfide (-S-S-) linkers are amongst the  
14 most appealing options in order to achieve a spatially and temporally controlled intracellular  
15 cleavage of cationic lipids, lipoplex disassembly, and NAs release. Some evidence suggests  
16 that reducible disulfide bonds in lipids undergo intracellular reduction owing to the presence  
17 of reducing agents (Zhang et al., 2012). Therefore, from the inception of the first cationic lipid  
18 containing a S-S linkage, namely 1,2-dioleoyl-sn-glycero-3-uccinyl-2-hydroxyethyl disulfide  
19 ornithine (DOGSDSO) (Tang and Hughes, 1998), an increasing number of disulfide-bearing  
20 lipids have been synthesized (Shirazi et al., 2011; Wetzer et al., 2001). To this aim, our group  
21 designed a SS14 bio-reducible *gemini* surfactant that has been used to shed light on the  
22 mechanism of action of redox-sensitive transfectants (Candiani et al., 2010, 2008). Of note,  
23 we found that the effectiveness of SS14 was strictly dependent on intracellular glutathione  
24 (GSH) levels.

25 Lipids bearing disulfide linkers have also been profitably used to deliver siRNAs and  
26 silence genes (M. Wang et al., 2014). In this regard, Gujrati *et al.* demonstrated that the use  
27 of the sulfur-containing amino acid cysteine in the linker domain did not only control the release  
28 of siRNA in the cytosol, but also contributed to the overall stability of the complex itself (Gujrati  
29 et al., 2014). Additionally, cysteine residues could be profitably used as the anchoring group  
30 to tether a given targeting moiety to the carrier (Wang et al., 2009).

31 On the other side, lipids with enzyme-cleavable linkers have been extensively exploited to  
32 achieve a sustained delivery of NAs into specific targets. The main advantage of such  
33 approach is that the amount of NAs released from lipoplexes depends on the enzyme  
34 concentration and localization (Fouladi et al., 2017). As an example, it has been shown that  
35 the lipid PEG-peptide-DOPE (PEG-PD) underwent disassembly because of substantial  
36 cleavage of the peptide moiety by means of the matrix metalloproteinase-2 (MMP-2), an  
37 enzyme specifically expressed at high levels at target sites (Terada et al., 2006). Comparable  
38 outcomes were found in other studies using similar vectors (Bruun et al., 2015; Hatakeyama  
39 et al., 2009; Koutroumanis et al., 2013).

40 The use of the cationic lipid backbones featuring photosensitive linkers represents a  
41 valuable alternative to the other environment-sensitive amphiphiles described herein above.  
42 In this context, Nagasaki and co-workers developed an array of cationic amphiphiles to  
43 ascertain the role of photocleavable (UV-sensitive) linkages on the lipoplex activity.  
44 Interestingly, they found that the UV-induced linker cleavage allowed NAs to escape from  
45 endocytic vesicles, such that their transfection efficiency was up to 20 fold-higher than that of  
46 Lipofectin (Nagasaki et al., 2003).

47

1 Together, these findings entail that each and every linker moiety has an impact on the  
2 stability of the lipoplexes, which, in turn, plays a role in tuning the cytotoxicity and the  
3 transfection efficiency of lipoplexes. Even though different kinds of linkers show specific pros  
4 and cons, biodegradable, environment-responsive moieties, such as carbamate and  
5 disulphide linkers, are the most promising candidates because giving rise to low cytotoxicity  
6 and high transfection efficiency.

### 7 8 **2.3. Tails**

9 The tail moiety is the hydrophobic domain of cationic lipids. Structure-activity relationship  
10 (SAR) studies have shown that non-polar tails play a role in the phase transition, and thus in  
11 the fluidity, overall stability and cytotoxicity of the resulting lipoplexes (Jones et al., 2013).  
12 Depending on the structure, hydrophobic tails are classified as aliphatic chains or cyclic  
13 (steroid-based) domains.

#### 14 15 **2.3.1. Aliphatic chains**

16 The aliphatic tails of cationic lipids are typically saturated (e.g., stearyl) or unsaturated  
17 (e.g., oleyl). Despite the number of chains displayed by the lipid, their length and the degree  
18 of unsaturation have been found to influence the transfection performances of the resulting  
19 lipoplexes (Jones et al., 2013), there is no general consensus as to which an ideal tail design  
20 should be (Felgner et al., 1994; T. Ren et al., 2000; Song et al., 1997).

21 As a general rule, the shorter the saturated chain of the cationic lipid, the **higher the**  
22 effectiveness. On this matter, the optimal chain length of aliphatic tails was unfortunately found  
23 to vary dramatically from study to study. Some authors concluded that short hydrocarbon  
24 chains, such as those composed of 10 to 14 carbon atoms, are the most effective in  
25 transfection (Gopal et al., 2006; Venkata Srilakshmi et al., 2002). On our side, we checked the  
26 effectiveness of an array of cationic lipids with hydrocarbon tails of various length. Of note, we  
27 found a bell-type transfection trend with an optimum performance corresponding to C<sub>14</sub>, while  
28 shorter and longer aliphatic tails were less effective (i.e., C<sub>14</sub> > C<sub>12</sub> > C<sub>10</sub> and C<sub>14</sub> > C<sub>16</sub> > C<sub>18</sub>)  
29 (Candiani et al., 2007).

30 Yet, the identification of the optimum number of aliphatic chains the cationic lipid should  
31 display to achieve the **optimized** transfection is still matter of debate. In fact, it is generally  
32 accepted that lipids with two hydrophobic chains, such as DOTMA, DOTAP, DOPSA, DORIE,  
33 DOGS and others, **are more effective in** transfection than single-tailed lipid **counterparts**.  
34 Nevertheless, their performances are largely dependent on factors other than the simple  
35 number of hydrophobic chains, such as geometrical and chemical features (Ewert et al., 2010).  
36 **A possible explanation as to why the transfection efficiency of two-tailed cationic lipids was**  
37 **high may rely** on their **potential to form** stable aggregates in aqueous solutions (Li et al., 2013;  
38 H. Wang et al., 2014). By contrast, single-chained cationic lipids are more prone to form  
39 unstable lipoplexes characterized by higher cytotoxicity and reduced transfection efficiency  
40 (Lv et al., 2006; Pinnaduwege et al., 1989). Of note, the combination of single- and double-  
41 tailed lipids to give mixed liposomes had a positive synergistic effect on the transfection  
42 efficiency (Li et al., 2013; Wu et al., 2016).

43 Although seldom used, multi-tailed lipids have shown some intriguing results in  
44 transfection (Byk et al., 1998; Gaucheron et al., 2002). In this regard, it has been recently  
45 shown that the cationic lipid bearing three saturated alkyl chains N-[6-amino-1-oxo-1-(N-  
46 tetradecylamino)hexan-(2S)-2-yl]-N'-{2-[N,N-bis(2-aminoethyl)-amino]ethyl}-2,2-  
47 ditetradecylpropandiamide (DiTT4), used in combination with DOPE, gave rise **to** very  
48 effective lipoplexes (Wölk et al., 2015b, 2015a).



1           Moreover, it has been shown that the symmetry of the two alkyl chains bound to the  
2 headgroup plays some role in the **behavior** of **two**-tailed cationic lipids (Chandrashekar et al.,  
3 2011; Hiwale et al., 2017; Le Corre et al., 2014; Wang and Macdonald, 2004). SAR studies  
4 revealed that the degree of asymmetry between the two tails strongly impacts the phase  
5 behavior of the resulting lipid as a consequence of the differences in the overall tail free volume  
6 (Zhang et al., 2011). Indeed, in **two**-tailed lipids with chains of different lengths, the packing  
7 density decreases, and voids created by the presence of shorter chains severely reduce the  
8 rigidity of the assembly overall, thus affording a greater intermembrane mixing (Le Corre et  
9 al., 2014). This is the reason why several authors **have suggested using** asymmetric lipids to  
10 attain **high** transfection efficiency (Dileep et al., 2001; Le Corre et al., 2014; Wang et al., 2006).

11           Unsaturated alkyl chains are also believed to increase the transfection performances of  
12 lipids because they are known to increase the membrane fluidity and display a good fusogenic  
13 behavior (Arpicco et al., 2004; Heyes et al., 2005). The effectiveness of lipoplexes containing  
14 unsaturated lipid tails depends on three variables, that is, the number of double bonds, their  
15 position along the chain and their configuration (Zhi et al., 2010). Even **though** few reports  
16 **have showed** a **direct** correlation between the degree of unsaturation and transfection  
17 efficiency (Inoh et al., 2010), it is generally accepted that **lipoplexes made of lipids with**  
18 **monounsaturated chains are the most efficient** in transfection (Arpicco et al., 2004; Delepine  
19 et al., 2000; Zhi et al., 2010; Zuhorn et al., 2002). **For the sake of comparison**, Loizeau and  
20 colleagues examined different cationic lipids with invariable heads but different hydrophobic  
21 tails, such as saturated, mono- and poly-unsaturated alkyl chains of different lengths, and  
22 found that C<sub>18</sub>-long, monounsaturated single-tailed amphiphiles were the most effective in  
23 terms of DNA condensation and transfection efficiency (Loizeau et al., 2013). Besides, the  
24 solid geometry of the unsaturated aliphatic chains is another important factor to be taken into  
25 account (Giacometti et al., 2017; Zhu et al., 2008). In this regard, **many** authors have shown  
26 that the *cis* configuration is the most effective in transfection (Obika et al., 2001; Zhu et al.,  
27 2008; Zhu and Mahato, 2010).

### 28 29           **2.3.2. Cyclic (steroid-based) domains**

30           Since the development of the popular DC-Chol (Gao and Huang, 1991), many other  
31 steroid-based transfectants have been designed (Kearns et al., 2008; Kim et al., 2014;  
32 Vigneron et al., 1996). Steroids in general, and cholesteryl specifically, are often used in place  
33 of aliphatic chains because inherently rigid, biodegradable (Martin et al., 2005; Zidovska et al.,  
34 2009), biocompatible (Choi et al., 2001; Lee et al., 2004), and fusogenic (Ohvo-rekila et al.,  
35 2002; Silviu, 2003).

36           Han *et al.* developed two novel Chol-based lipids, i.e., cholesteryloxypropan-1-amine  
37 (COPA) and cholesteryl-2-aminoethylcarbamate (CAEC), to efficiently deliver siRNA  
38 molecules into cells (Han et al., 2008), while Bhattacharya's group synthesized a series of  
39 *gemini* Chol-based **cationic** surfactants **that displayed transfection efficiencies similar to those**  
40 **of the single-tailed analogues and to the gold standard Lipofectamine** (Bajaj et al., 2007;  
41 Biswas et al., 2011).

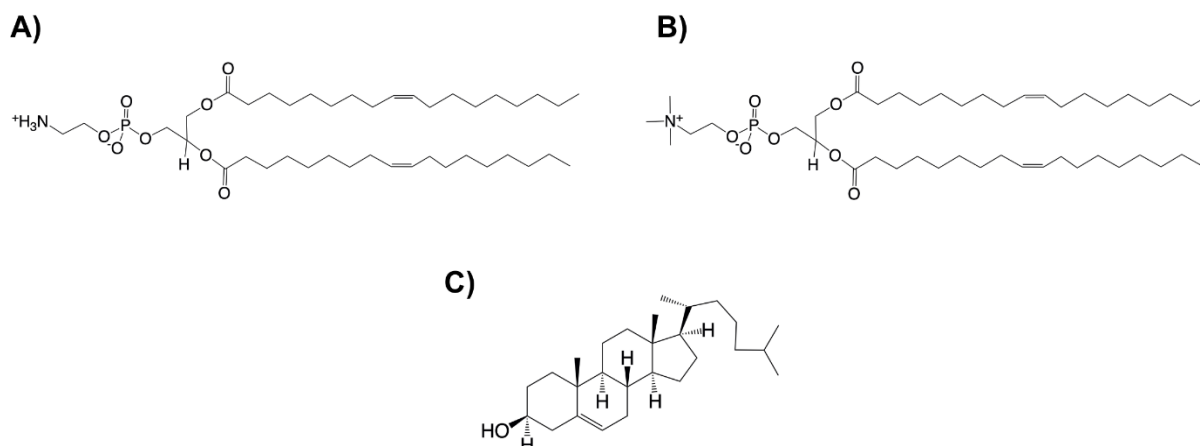
42           Besides, despite Chol has been the most employed non-aliphatic domain so far, other  
43 steroids, such as vitamins (Tan Ren et al., 2000), bile, cholestane and lithocholic acid  
44 (Fujiwara et al., 2000; Walker et al., 1996), have been used to synthesize cationic amphiphiles  
45 for gene delivery applications. **For instance, vitamin D<sub>2</sub> and D<sub>3</sub> have been used to synthesize**  
46 **an array of lipid transfectants as effective as DC-Chol** (Tan Ren et al., 2000). **More recently,**  
47 **other** studies pointed to the use of  $\alpha$ -tocopherol, a derivative of vitamin E, to synthesize  
48 cationic lipids with superior transfection properties (Kedika and Patri, 2012, 2011; Zheng et

1 al., 2016). Because similar to Chol, bile acids have **also** been used with some success (Walker  
2 et al., 1996).

3  
4 Taken together, these findings disclose both aliphatic and cholesterol-based tails as  
5 suitable hydrophobic domains to design cationic lipid transfectants. In this regard, there is a  
6 consistent body of evidence that the single-tailed cholesterol-based motif and two-tailed  
7 monounsaturated aliphatic chains are the most suited lipophilic moieties to design cationic  
8 lipids for gene delivery.

### 9 10 **3. Helper lipids**

11 Although sole cationic lipids have been shown to successfully deliver NAs, they are often  
12 combined with helper lipids, also called co-lipids, which are typically zwitterionic lipids such as  
13 DOPE or 1,2-dioleoyl-sn-glycerol-3-phosphatidylcholine (DOPC), **among others**, to increase  
14 their effectiveness. **Indeed**, helper lipids assist the formation of different supramolecular  
15 assemblies that strongly affect the colloidal stability of lipoplexes by promoting their interaction  
16 with cell membranes (Balazs and Godbey, 2011; Buck et al., 2019; Du et al., 2014; Mochizuki  
17 et al., 2013).



19  
20 **Figure 4.** Chemical structure of different helper lipids, namely: **A)** DOPE; **B)** DOPC; **C)** Chol.

21 DOPE consists of a relatively small phosphoethanolamine headgroup bound to two bulky  
22 and unsaturated oleyl chains by means of ester linkages (**Figure 4A**), and acts as a fusogenic  
23 lipid. Quite for this reason, it has been frequently incorporated in early designs of lipoplexes  
24 in order to achieve an unstable geometry at acidic pH and enable the endo-lysosome  
25 destabilization, and the consequent NAs release (Hoekstra et al., 2007). Mochizuki and  
26 colleagues revealed that DOPE-containing lipoplexes underwent conformational changes  
27 when the pH was lowered from 7 to 4, as it occurs in the late endosomes environment  
28 (Mochizuki et al., 2013). Due to the above mentioned **behavior**, DOPE has been added to  
29 several lipid formulations which are on the market, such as Lipofectin (a lipid formulation  
30 consisting of 1:1 (w/w) mixture of DOTMA and DOPE) and Lipofectamine (a 3:1 (w/w) mixture  
31 of DOSPA and DOPE) (Dalby et al., 2004; Wang et al., 2018).

32 DOPC is a lipid with a zwitterionic behavior given by the occurrence of both an anionic  
33 phosphate and a cationic choline moiety (**Figure 4B**) (Bhattacharya and Bajaj, 2009). It is  
34 inherently prone to give rise to stable structures, which are considered to be less effective in  
35 transfection than those containing DOPE (May et al., 2000). To shed more light on the effects  
36 of helper lipids, some authors investigated the transfection behavior of DOTAP in combination  
37 with DOPE or DOPC and, as hypothesized, they found out the **superior** effectiveness of the

1 former formulation (Hattori et al., 2005). In this regard, it was found that DOPE-containing  
2 lipoplexes exhibited quick endosomal trafficking and DNA accumulation within the nucleus,  
3 while lipoplexes containing DOPC settled into the late endo-lysosomes (Du et al., 2014; Zhang  
4 and Anchordoquy, 2004; Zylberberg et al., 2017).

5 Chol (**Figure 4C**) has also been used as **the** helper lipid in many formulations. Chol is a  
6 natural, waxy steroid found in all animal cell membranes. In nature, the hydroxyl group of each  
7 Chol molecule interacts with the water surrounding the membrane, while the bulky steroid and  
8 the hydrocarbon chains are embedded within the membrane, alongside the non-polar fatty-  
9 acid chains of the other lipids. Through the interaction with the fatty-acid chains of  
10 phospholipids, Chol increases membrane packing and allows retaining membrane integrity  
11 (Koynova and Tenchov, 2009). Besides, being Chol an uncharged amphiphile, it does not  
12 interact directly with NAs, but rather it supports cationic lipids to interact with them (Xu and  
13 Anchordoquy, 2008). In addition, it has been reported that Chol may **favor the** interactions with  
14 plasma and endosomal membranes (Pozzi et al., 2012). All these findings support the idea  
15 that the formulation of cationic lipids with Chol may improve the overall transfection  
16 performances of lipoplexes (Betker et al., 2013; Dabkowska et al., 2012; Faneca et al., 2002).

17 Although it is commonly accepted that some cationic lipids work exclusively with specific  
18 helper lipids and not with others, Mukherjee *et al.* have investigated the possible effect on  
19 transfection of the co-presence of common co-lipids (Mukherjee et al., 2005). Of note, it turned  
20 out that, when acting in synergy, the helper lipids DOPE, DOPC, and Chol improved the gene  
21 transfer properties of some **newly synthesized** cationic lipids **with different aliphatic chain**  
22 **lengths** but failed to do so to the same extent when taken individually. Similar results were  
23 confirmed by other authors who used mixtures of **the** cationic **lipid DDAB** and **the** helper lipids  
24 **DOPE, DOPC, Chol and two kinds of phosphatidylcholines** (Safari and Hosseinkhani, 2013).

25 In light of such promising results about the use of co-lipids to improve the transfection  
26 performances of cationic lipids, recent studies have focused on the design of novel helper  
27 lipids, for instance bearing triggerable elements (Le Gall et al., 2014; Réthoré et al., 2007;  
28 Zheng et al., 2015). Just as an example, Zheng and colleagues synthesized the zwitterionic  
29 amphiphile trans-2-aminoacyclohexanol (TACH) and used it in combination with DOTAP in an  
30 attempt to improve its gene delivery efficiency. Due to the pH-responsiveness displayed by  
31 the former molecule, the formulation of DOTAP with TACH proved to be more effective than  
32 the conventional DOTAP:DOPE and DOTAP:Chol mixtures (Zheng et al., 2015).

33  
34 **Overall, even though different kinds of helper lipids have been found to enhance to some**  
35 **extent the performance of cationic lipids, DOPE and Chol have emerged as the most widely**  
36 **used because they favor the interaction of the lipoplexes with the cellular membranes.**

#### 37 38 **4. Structure and properties of lipoplexes: from complexation to transfection** 39 **efficiency**

40 The performances of a given vector are definitely affected by the chemical features of the  
41 amphiphile, that is, the chemical structure of each domain and the interplay among them.

42 Relying on the composition of the lipid, different supramolecular structures can be  
43 obtained. When these are mixed with NAs, things get even trickier. In the next sections, the  
44 interplay between lipid chemistry, some rearrangements that give rise to supramolecular  
45 assemblies, and how these together affect the final transfection outcomes are discussed in  
46 some depth. Specifically, by focusing on the steps that lead to complexation and on the factors  
47 that influence the structural and physico-chemical features of the resulting lipoplexes (i.e.,  
48 charge ratio (CR), temperature and complexation buffer), we seek to highlight how each and

1 every feature affects the ability of lipoplexes to overcome cellular barriers and achieve  
2 successful gene transfer.

#### 3 4 **4.1. Cationic lipids: from structure to aggregation phase**

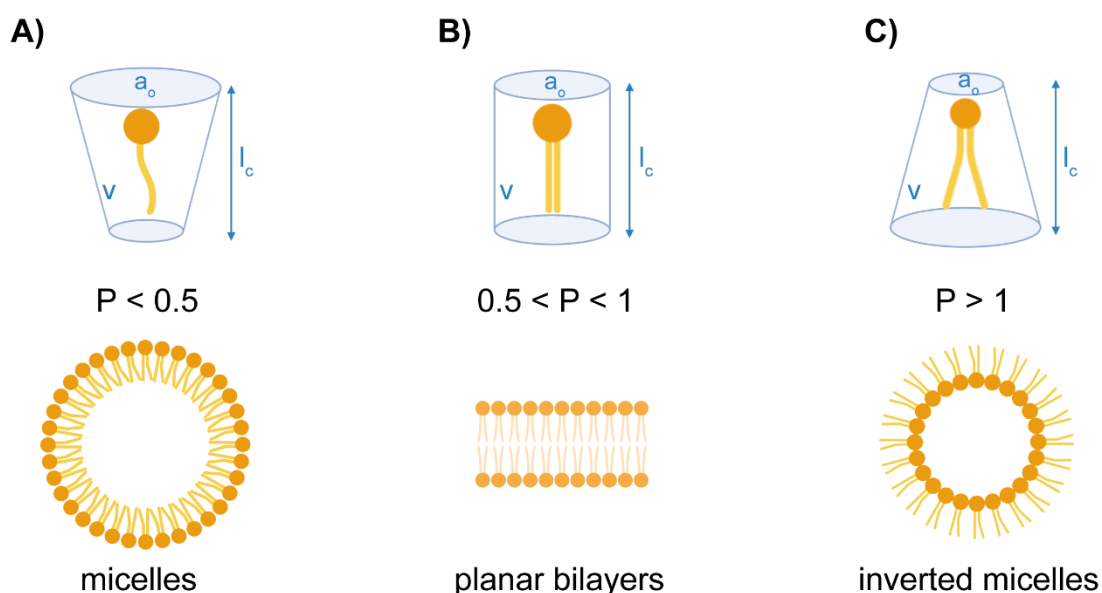
5 When dispersed in water at a certain concentration above their critical micellar  
6 concentration (CMC), amphiphiles naturally self-assemble into thermodynamically stable  
7 vesicles, which are the result of some structural rearrangements that minimize the exposure  
8 of the hydrophobic moieties to the protic solvent. Depending on the geometrical packing  
9 constraints imposed by hydrophilic and hydrophobic moieties that are specific to each lipid,  
10 different supramolecular assemblies have been proposed. An easy way to predict the  
11 conformation of a given amphiphile is by means of the so-called packing parameter (P), which  
12 is defined according to the Eq. 1 (Hsu et al., 2005):

$$13 \qquad P = \frac{v}{a_0 \times l_c} \qquad \text{(Eq. 1)}$$

14  
15 where:

16 v is the molecular volume of the hydrocarbon tails;  
17  $a_0$  is the surface area occupied by the polar headgroup;  
18  $l_c$  is the length of the hydrophobic chain(s).

19  
20  
21 In short, this equation emphasizes the relevance of the ratio between the volume occupied by  
22 the hydrophobic region and that of the hydrophilic domains. Lipids with  $P < 0.5$  are cone-  
23 shaped (e.g. lysophosphocholine, LPC) (Kang et al., 2016) because they have bulky  
24 headgroups with a single short hydrocarbon chain (**Figure 5A**), and do associate in micelles  
25 with a positive membrane curvature. Conversely, lipids bearing headgroups which exhibit  
26 about the same cross-sectional area than hydrophobic tails ( $0.5 < P < 1$ ) are referred to as  
27 cylindrical-shaped lipids (e.g., DOTAP and DOPC) (**Figure 5B**) and are prone to assemble  
28 into a lamellar structure, that is, a bilayer with nearly zero curvature (Majzoub et al., 2016).  
29 Conversely, inverted cone-shaped lipids have larger hydrophobic moieties with respect to  
30 polar heads such that  $P > 1$  (e.g., DOPE) (**Figure 5C**). They associate with each other to give  
31 inverted hexagonal phases (Cullis and Hope, 1986; Pezzoli et al., 2012).



1 **Figure 5.** Schematic representation of the molecular shape that cationic lipids may have, and the  
 2 supramolecular structure they may form, depending on the packing parameter ( $P$ ). Specifically,  $a_o$  is  
 3 referred to the area of the polar headgroup,  $l_c$  represents the length of the hydrophobic domain, while  $v$   
 4 refers to the hydrocarbon volume. Depending on the  $P$  value, cationic amphiphiles are depicted by **A)**  
 5 cone-like geometry, **B)** cylindrical shape, and **C)** inverted cone geometry. They may aggregate to give  
 6 rise to the formation of micelles, planar bilayers, and inverted micelles, respectively.  
 7

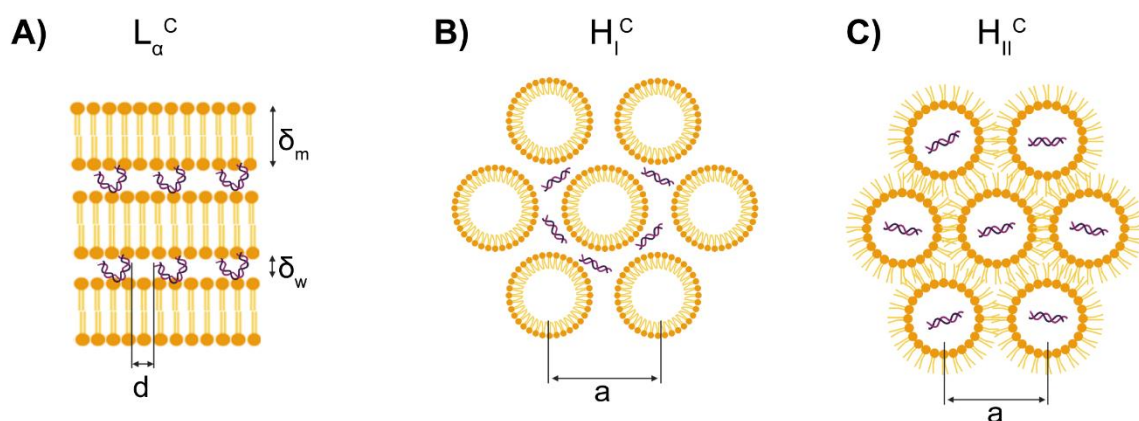
8 Despite the prediction of the 3D structure of lipids which is relatively simple, the  
 9 conformational changes occurring just after mixing NAs and lipids are not as trivial to predict  
 10 (Koynova and Tenchov, 2009). Lipoplexes are usually obtained by adding NAs to the cationic  
 11 lipids in order to enable the natural assembly of the two components. **So far, a number of**  
 12 **studies have shown the ability of different cationic lipids to bind and condense NAs of various**  
 13 **size, including DNA molecules in the form of pDNA and oligonucleotides (Caracciolo and**  
 14 **Amenitsch, 2012; Koynova and Tenchov, 2010; Meidan et al., 2000; Tros de Ilarduya et al.,**  
 15 **2010; Wang et al., 2015; Weisman et al., 2004), and RNA molecules, such as siRNA and**  
 16 **mRNA (Guevara et al., 2020; Midoux and Pichon, 2014; Semple et al., 2010; Zhang et al.,**  
 17 **2007). Therefore, when mixing NAs with cationic lipids, the size and the 3D arrangement of**  
 18 **the former may affect the physico-chemical features and the supramolecular structure of the**  
 19 **resulting complexes (Ewert et al., 2010; Rao, 2010; Scholz and Wagner, 2012).**

20 Although conceptually simple, lipoplex formation is a multi-step and multi-length scale  
 21 process that relies upon the temperature, volume and ionic strength of the medium, and  
 22 relative concentrations **and types** of NAs and cationic lipids (Fuj and Sakura, 2012; Ilies et al.,  
 23 2002; Tros de Ilarduya et al., 2010). **Complexation** primarily consists of two major phases: i)  
 24 a long-lasting but abrupt (i.e., in the order of milliseconds) interaction between the anionic  
 25 phosphates of NAs and the cationic headgroups of cationic lipids. This step is spontaneous  
 26 and driven by the entropic gain associated to counterions release in solution (Gao et al., 2010;  
 27 **Sennato et al., 2005**); ii) a slower, endothermic process of irreversible rearrangement and  
 28 stabilization of the lipoplex itself (Dan, 2015; Kang et al., 2016; Koynova and Tenchov, 2009).  
 29 Biophysical studies with small-angle X-ray scattering (SAXS) and differential scanning  
 30 calorimetry (DSC) revealed that the binding of cationic lipids to NAs results in lipid  
 31 rearrangement and mixing (Mrevlishvili et al., 1998; Wasungu and Hoekstra, 2006). During  
 32 this step, the hydrophobic portions of cationic lipids may be provisionally exposed to water



1 and rearrange into unstable conformations. In turn, these undergo rearrangement by means  
2 of hydrophobic interactions (Matulis et al., 2002) to give different thermodynamically favored  
3 assemblies (Caracciolo and Amenitsch, 2012; Fuj and Sakura, 2012), such as spaghetti-and-  
4 meatballs, lamellae and rod-like structures (Elouahabi and Ruyschaert, 2005). **Of note, the**  
5 **organization of lipids and NAs in specific 3D architectures (Figure 6) impacts the ability of**  
6 **lipoplexes to overcome some delivery barriers, and thus their transfection efficiency (Ma et al.,**  
7 **2007; Safinya et al., 2011).**

8 Broadly speaking, complexes made with cationic lipids and NAs may have two typical  
9 structures, namely the (multi)lamellar phase ( $L_{\alpha}^C$ ) (Figure 6A) and the hexagonal phase ( $H_I^C$ ,  
10  $H_{II}^C$ ) (Figures 6B and 6C).  
11



12  
13 **Figure 6.** Schematic representation of the supramolecular structures of lipoplexes: **A)** lamellar phase  
14 ( $L_{\alpha}^C$ ); **B)** hexagonal phase ( $H_I^C$ ) and **C)** inverted hexagonal phase ( $H_{II}^C$ ).

15  $L_{\alpha}^C$  phase (Figure 6A) typically occurs when using cylindrical-shaped lipids (Figure 5B).  
16 It is composed of different lipid bilayers, with NAs intercalated among them. **Studies carried**  
17 **out by means of cryo-transmission electron microscopy (cryo-TEM) revealed that the**  
18 **complexation of lipids and NAs into multilamellar assemblies starts with the absorption of NAs**  
19 **on pre-formed liposomes, followed by the clustering of different unilamellar structures. The**  
20 **high deformation and packing pressure arising from the electrostatic interaction of one side of**  
21 **the bilayer with NAs ultimately lead to the rearrangement of the bilayer itself and the formation**  
22 **of multi-lamellar assemblies (Huebner et al., 1999). The NA strands present in the interlamellar**  
23 **gaps lie parallel from each other, and at a repeatable distance  $d$  that depends upon cationic**  
24 **lipids and the eventual presence of helper lipids. The interlayer spacings are defined by the**  
25 **membrane thickness ( $\delta_m$ ) and the water gap ( $\delta_w$ ), which are about 5 nm and 2.5 nm,**  
26 **respectively. Depending on the packing level, which is dictated by the NA content, the distance**  
27  **$d$  between NA molecules is from 2.5 nm and 5 nm. Of note, even if such bilayers have a quasi-**  
28 **zero curvature, some buckling may occur when interacting with NAs (Safinya, 2001; Safinya**  
29 **et al., 2011). Lipoplexes displaying  $L_{\alpha}^C$  phase have been found stable in both the intracellular**  
30 **and in the extracellular environments, that is, they are little prone to fuse with cellular**  
31 **membranes, such that their transfection efficiency is generally low (Ma et al., 2007).**

32 In the hexagonal phase  $H_I^C$  (Figure 6B), the DNA molecules are embedded in the aqueous  
33 voids of the hexagonal lipid matrix. Due to the constraints of lipid chain packing, lipoplexes  
34 adopting a  $H_I^C$  phase are usually composed of cone-like lipids (Figure 5A) that form a  
35 honeycomb-like structure made up of micelles with a constant distance  $a$  of about 8.15 nm  
36 between the centres (Kang et al., 2016).

1 Conversely, the inverted hexagonal phase  $H_{II}^C$  (**Figure 6C**) consists of DNA rods coated  
2 with a lipid monolayer arranged on a hexagonal lattice. While the hydrophobic portions of the  
3 inverted micelles interact with each other, the positively charged headgroups engage with  
4 NAs. With respect to  $H_{II}^C$ , the distance between the centres  $a$  is lower ( $a = 6.74$  nm) (Kang et  
5 al., 2016). Besides, this phase is obtained as the result of the arrangement of inverted cone  
6 cationic lipids (**Figure 5C**), and it is favored in the presence of the helper lipid DOPE (Wasungu  
7 and Hoekstra, 2006) that gives rise to packing constraints (Dan, 2018; Gruner, 1989). **Lipid/NA**  
8 **complexes featuring  $H_{II}^C$  phase are less stable. Indeed, they have high fusogenicity, that is,**  
9 **NAs are more easily released inside the cell and the transfection efficiency is increased as a**  
10 **result (Ewert et al., 2005; Giacca, 2010; Koynova et al., 2006; Lin et al., 2000; Ma et al., 2007).**

11 Despite the lamellar and hexagonal phases are the most common and researched  
12 supramolecular assemblies, recent studies revealed that lipoplexes may also take a cubic  
13 phase ( $Q_{II}^C$ ). Such metastable cubic mesophase confers lipoplexes some fusogenic behavior,  
14 which impacts the overall transfection efficiency (Dittrich et al., 2018; Leal et al., 2010;  
15 Mcloughlin and Impørør-clerc, 2004).

16 It is worthy of note that the information provided herein above are specific to the use of  
17 DNA. Because siRNAs are obviously shorter, less rigid, and have higher rotational and  
18 translational degrees of freedom than large DNA molecules, siRNA-bearing lipoplexes take  
19 less time to reach the equilibrium, and feature more fluid bilayers (Bouxsein et al., 2007; Kang  
20 et al., 2016).

## 22 **4.2. Shaping lipoplexes: factors affecting their behavior**

23 The **stability and** transfection performances of lipoplexes are strongly affected by a variety  
24 of formulation factors. **Therefore, in order to improve the effectiveness of lipoplexes, some**  
25 **parameters have** to be taken into account, **such as** i) the lipid-to-NA ratio (i.e., in other words,  
26 the CR), which was found to affect the charge density of the complexes, their dimensions,  
27 **shape** and overall colloidal stability; ii) the environmental conditions, that is, the temperature,  
28 the ionic strength and **the** pH of the aqueous solution in which lipoplexes are prepared. These  
29 impact the complexation kinetic as well.

### 31 **4.2.1. Lipid-to-NA ratio (charge ratio)**

32 The charge ratio (CR) represents the mole ratio between cationic moieties, such as the N  
33 atoms, of the lipid headgroup and the negative charges brought by the phosphate groups of  
34 the NAs to be delivered. This means that at CR 1 there should be a complete charge  
35 neutralization such that NAs are fully complexed. Although theoretically reasonable, this  
36 seldom happens in practice because of some steric hindrance between NAs and cationic  
37 lipids, and because of some other geometrical constraints. A slight-to-moderate excess of  
38 positive charges is thus needed in order to get NAs completely buried within lipoplexes  
39 (Elouahabi and Ruyschaert, 2005). In light of this, it is apparent that the CR is probably the  
40 most prominent factor that allows to fine-tune the effectiveness of lipoplexes through the  
41 modulation of their colloidal stability. In order to emphasise how the CR may affect the  
42 formation of lipoplexes with different behavior, Garidel and Funari compared lipoplexes made  
43 with the cationic lipid DC-Chol and DNA at different lipid: DNA weight-to-weight (w/w) ratios.  
44 Of note, only in the presence of a large excess of cationic lipid with respect to NAs, stable  
45 non-lamellar structures were achieved (Garidel and Funari, 2006).

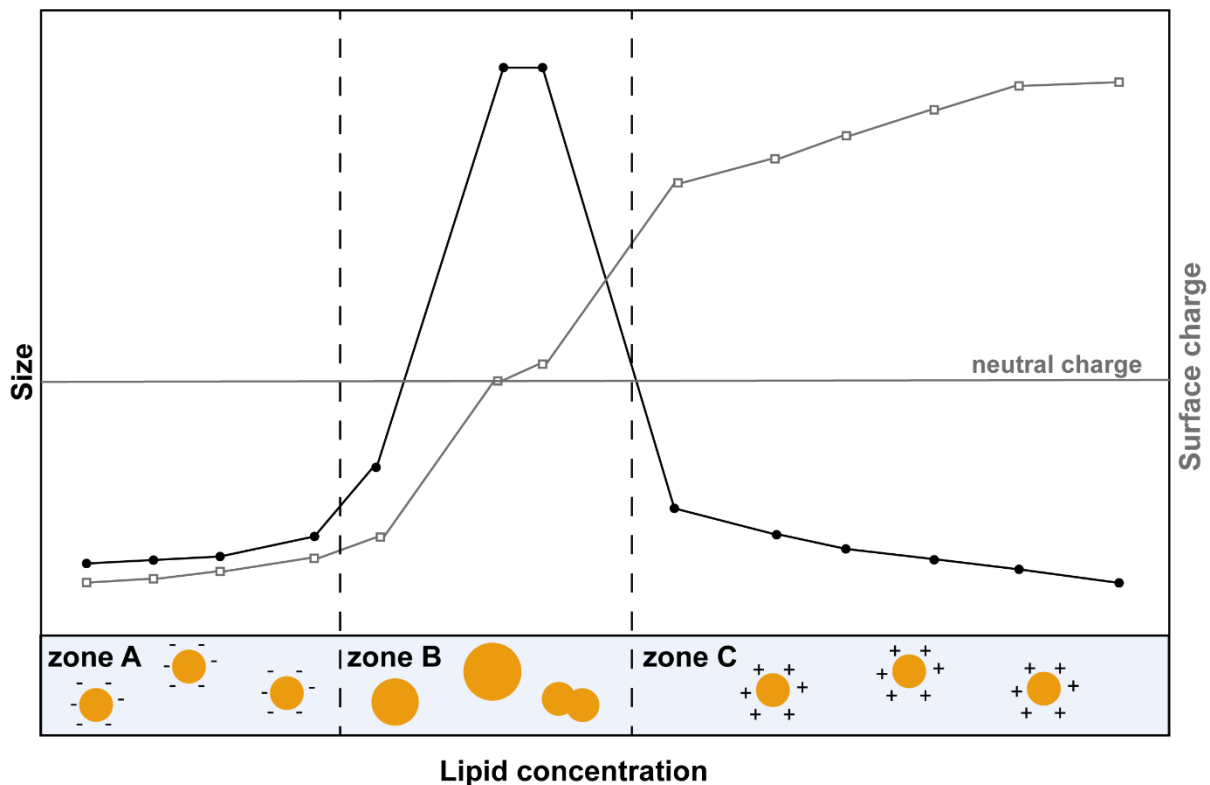
46 The CR is also known to impact the complexation kinetics: while lipoplexes at high CR are  
47 known to reach quickly a steady-state equilibrium, those formed at lower CR require longer



1 time to rearrange and reach stability (Dan, 2015). Besides, although the complexation is  
2 carried out faithfully following the general scheme mentioned above, even subtle changes in  
3 the experimental protocol adopted have a **strong** impact on the lipoplex formation (Sennato et  
4 al., 2005; Zuzzi et al., 2007) and behavior (Rakhmanova et al., 2004). **The process of lipoplex**  
5 **formation has been thoroughly investigated so far. It has been shown that when anionic NAs**  
6 **are added to the cationic lipids, the latter rapidly bind to the former molecules due to counterion**  
7 **release (Harries et al., 2013). On the other hand,** if we add cationic lipids to NAs, instead of  
8 *vice versa*, the complexation takes longer to happen and leads to the wrapping of NAs by  
9 preformed lipid aggregates, thus limiting somewhat the intimate lipid mixing and the structural  
10 rearrangements that may happen within the lipoplex (Wasungu and Hoekstra, 2006).

11 The CR also affects the physico-chemical features of the particles, namely their size  
12 (hydrodynamic diameter,  $D_H$ ), and their surface charge (zeta-potential,  $\zeta_P$ ). Of note, since the  
13 cellular uptake of particles is a size- and charge-dependent process (Foroozandeh and Aziz,  
14 2018), small and positive complexes were reported to be the most **stable and** effective in  
15 transfection **experiments** (Tros de Ilarduya et al., 2010). As a general rule, the higher the CR,  
16 the greater the  $\zeta_P$ , and the lower the size of lipoplexes (Buck et al., 2019). This means that  
17 lipoplexes show specific colloidal stability depending on the CR, as schematically depicted by  
18 the three-zones colloidal stability model reported in **Figure 7** (Bartreau et al., 2008; Pitard,  
19 2002; Sainlos et al., 2007; Tranchant et al., 2004). In more detail, **zone A (i.e., low lipid**  
20 **concentration)** is comprised of colloidally stable but ineffective complexes that are negatively  
21 charged because there are still some uncondensed NA molecules surrounding the lipoplexes.  
22 **The electrostatic repulsive forces prevent lipoplexes from aggregation. Zone B** consists of  
23 large and colloidally unstable lipoplexes with a barely neutral surface charge. **Lipoplexes**  
24 **obtained at CRs close to the isoelectric point (Figure 7) (i.e., it is where the opposite charges**  
25 **of the polyelectrolyte (NA) and the cationic surfactant (lipid) become neutralized and the**  
26 **overall charge of the assembly is neutral) may interact with each other and form larger**  
27 **aggregates (Faneca et al., 2002). By increasing the lipid concentration (i.e., the CR), the “re-**  
28 **entrant condensation” and overcharging phenomena take place (Bordi et al., 2009; Grosberg**  
29 **et al., 2002; Sennato et al., 2005), so that zone C** includes colloidally stable and effective  
30 suspensions constituted by positively charged, **small** lipoplexes that strongly repel each other.  
31 This implies that small variations in the amount of cationic lipids used to prepare lipoplexes  
32 have a tremendous effect on their colloidal stability, and thus on their ultimately effectiveness  
33 as gene delivery vectors.

34



1  
2 **Figure 7.** Schematic representation of the colloidal stability model of lipoplexes, which depends on their  
3 size (black full dots) and overall surface charge (grey empty squares) as a function of the lipid  
4 concentration. Specifically, *zone A* refers to stable lipoplexes with uncomplexed NAs, and thus negative  
5 surface charge and small size; lipoplexes in *zone B* are neutral and colloidally unstable, such that they  
6 tend to aggregate in cluster-like particles with bigger size; complexes in *zone C* are stable, positively  
7 charged, and small due to 're-entrant condensation' and overcharging phenomena. The latter are the  
8 most effective in transfection.

#### 9 10 **4.2.2. Environmental conditions**

11 Being complexation a thermodynamically spontaneous process, environmental cues, such  
12 as the temperature and the salt concentration, have a dramatic influence on the cationic lipids-  
13 NAs interactions (Muthukumar, 1986). Some evidences showed how a rise in temperature  
14 could induce a looser packing of lipoplexes (Silva et al., 2012). A mechanistic explanation of  
15 this phenomenon relies on the different conformations that the NAs can take as a function of  
16 the temperature. In practice, the double stranded DNA is more relaxed at temperature  $\approx 40$  °C  
17 than the conventional super-coiled conformation found at lower temperatures (Tse-Dinh et al.,  
18 1997). Moreover, the strength of the interaction between NAs and lipids proved to be inversely  
19 related with temperature, such that when the temperature rises the binding is weaker (Matulis  
20 et al., 2002).

21 Likewise, temperature variations also affect the phase behavior of lipoplexes (Dan and  
22 Danino, 2014). Because the transition from  $L_{\alpha}^C$  to  $H_{II}^C$  was found to be a temperature-favored  
23 process (Scarzello et al., 2005b), inverted hexagonal  $H_{II}^C$  structures are more likely to occur  
24 when heating lipoplexes because  $\delta_m$  and  $\delta_w$  of the lamellar conformation consistently decrease  
25 (Pozzi et al., 2006).

26 The pH and the ionic strength of the medium in which complexation takes place are just  
27 as important. It has been reported that a neutral-to-slightly acidic environment is usually  
28 preferred to deprotonate NAs and protonate lipids at once (Buck et al., 2019). On the other  
29 hand, the ionic strength of the complexation medium, in other words, the concentration and  
30 the kinds of ions competing for absorption play a role in the final assembly of lipoplexes.  
31 Indeed, both NAs and lipids have to be charged and need to exchange counterions with the

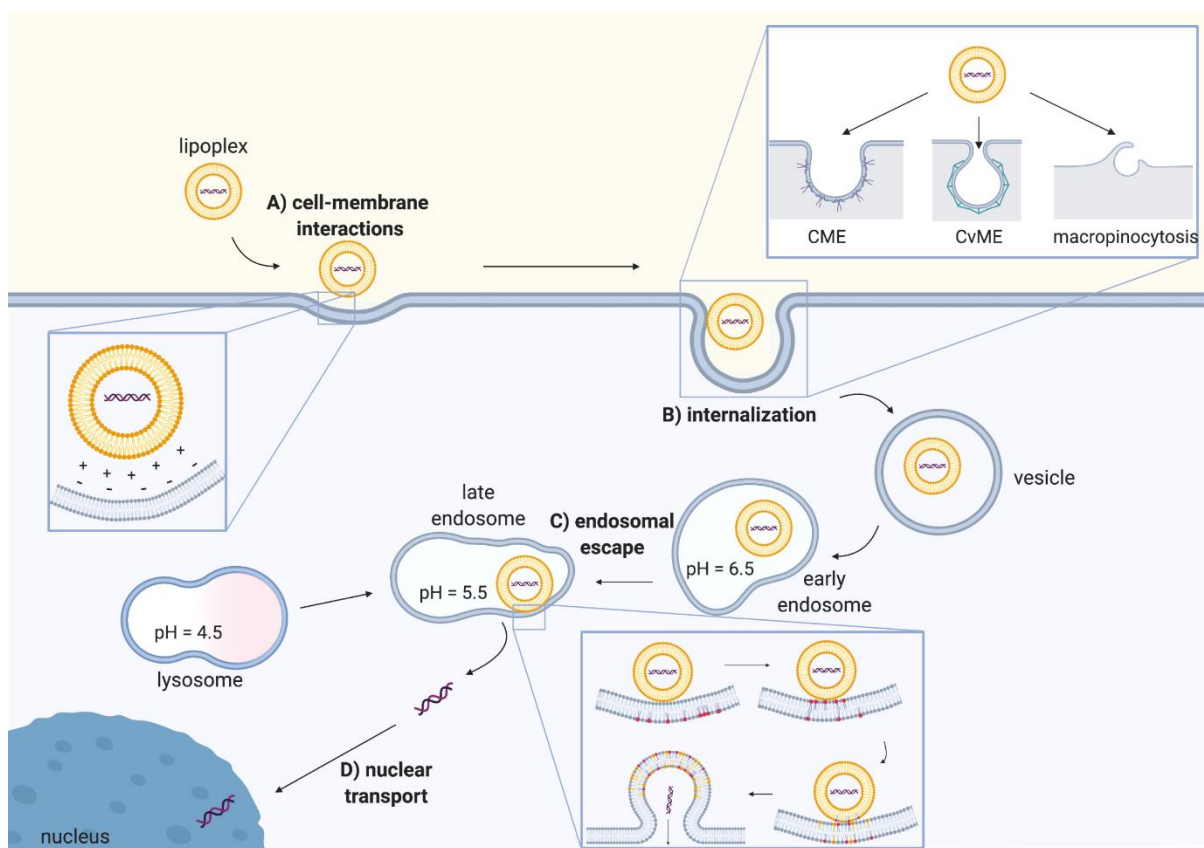
1 solution (e.g., 0.1 M NaCl) in order that complexation takes place (Harries et al., 2013).  
2 Nonetheless, a further increase in salt concentration (i.e.,  $\approx 0.4$  M NaCl) may hamper the  
3 counterion release, and complexation becomes impaired (Sennato et al., 2016; Tranchant et  
4 al., 2004; Zuidam and Barenholz, 1998).

5 Moreover, an increase in the ionic strength has also been found to trigger  $L_{\alpha}^C$  to  $H_{II}^C$  phase  
6 transition (Scarzello et al., 2005a) and results in the aggregation of lipoplexes (Bordi et al.,  
7 2009).

8

### 9 4.3. Cell-lipoplex interactions and trafficking

10 The successful delivery of NAs within the cells by means of non-viral vectors is hampered  
11 by a wide number of rate-limiting steps, namely the interaction of lipoplexes with the cell  
12 surface, their internalization, the release of the genetic cargo from endosomes and, when the  
13 delivery involves the DNA, its transfer into the nucleus (**Figure 8**) (Pezzoli and Candiani,  
14 2013).



15

16 **Figure 8.** Schematic representation of NAs delivery into cells mediated by cationic lipids. **A)** First,  
17 lipoplexes bind to the cell membrane through electrostatic interactions. **B)** Depending on their physico-  
18 chemical features, lipoplexes are internalized by means of different endocytic pathways, namely  
19 clathrin-mediated endocytosis (CME), caveolae-mediated endocytosis (CvME) or macropinocytosis. **C)**  
20 Once trapped within the endosome, lipoplexes are able to interact and fuse with anionic membrane  
21 lipids, ultimately leading to the release of the NAs in the cytosol. **D)** In case of DNA delivery, the delivery  
22 pathway ends with the transport of DNA molecules within the nucleus.

23 Therefore, the first hurdle that stands in the way of transfection is the binding of complexes  
24 to cell membrane (**Figure 8**, step **A**). It is generally believed that cationic lipoplexes interact  
25 with the anionic plasma membrane by means of electrostatic interactions. Although a net  
26 positive charge of lipoplexes was shown to enable their binding with the cell membrane, it is

1 just as true that the cationicity of lipoplexes is also responsible for their interaction with  
2 extracellular macromolecules, such as serum proteins (Zelphati et al., 1998; Zhang and  
3 Anchordoquy, 2004). In fact, serum proteins interact instantaneously and closely with  
4 lipoplexes (Simberg et al., 2005) and form the so-called protein corona. It has been shown  
5 that the effects of such a rich protein layer(s) on the ultimate stability and efficacy of lipoplexes  
6 are dependent on the serum protein content (Quagliarini et al., 2020): the presence of protein  
7 corona formed at low protein concentrations allows overcoming the electrostatic repulsion  
8 between lipoplexes, thus promoting their aggregation (Caracciolo et al., 2010). In turn, this  
9 was shown to lead to high transfection efficiency and low cytotoxicity (Masotti et al., 2009;  
10 Pezzoli et al., 2017; Rejman et al., 2004). On the other hand, protein corona formed at high  
11 protein concentrations induces the neutralization of the cationic charge of the lipoplexes. This  
12 resulted in the minimization of the electrostatic interactions with plasma membrane and/or the  
13 early release of the genetic cargo because of lipoplex destabilization (Maiolo et al., 2018).  
14 While most of the investigators agree that the lipoplex stability and functions are adversely  
15 affected by the presence of serum, little attention has been paid as to how the adsorption of  
16 specific proteins might be affected by some formulation parameters. In this light, the presence  
17 of neutral Chol in lipid formulations has been found to loosen the electrostatic interactions  
18 between cationic lipids and anionic serum proteins, thus improving their stability in the  
19 extracellular fluids, cellular uptake and transfection efficiency (Faneca et al., 2002; Zhang and  
20 Anchordoquy, 2004).

21 Once bound to the cell surface, lipoplexes must enter the cell (Figure 8, step B). Basically,  
22 this must be accomplished by passive or active (e.g., receptor-mediated) transport throughout  
23 the cell membrane. In the first and simplest case, lipoplexes fusion with the plasma membrane  
24 was suggested as a way to deliver NAs directly into the cytoplasm. It has been shown that a  
25 way to facilitate lipoplex-cell membrane fusion is through the use of helper lipids, such as Chol  
26 and DOPE (Buck et al., 2019; Zuhorn et al., 2005). Still, some experimental evidence supports  
27 the idea that the vast majority of lipoplexes are taken up by cells through endocytic pathways.  
28 Endocytosis, that is, the way cells internalize macromolecules and solutes by means of  
29 membrane-bound vesicles, is the main mechanism responsible for the internalization of non-  
30 viral vectors into cells (Cooper, 2000; Khalil et al., 2006). Notably, endocytosis can be  
31 classified in i) macropinocytosis, ii) clathrin-mediated endocytosis (CME) and iii) caveolae-  
32 mediated endocytosis (CvME) (Conner and Schmid, 2003; Lamaze and Schmid, 1995). After  
33 initiation of the endocytic site, the cargo is recruited, the membrane undergoes reshaping and  
34 scission (Peetla et al., 2015). Generally speaking, endocytic pathways differ in the composition  
35 of the coat (if any), in the size of the vesicles, and in the fate of the internalized particles (for  
36 further information concerning the uptake mechanisms please refer to (Khalil et al., 2006)).  
37 The internalization route of lipoplexes strongly depends on the size of the complexes (Jones  
38 et al., 2013; Rejman et al., 2006). As a rule of thumb, particles with dimensions of ~ 200 nm  
39 are typically internalized via clathrin-coated pits (CME), while larger particles with a size ~ 500  
40 nm undergo CvME. By using inhibitors of specific endocytic routes, Rejman *et al.* showed that  
41 the uptake of DOTAP-containing lipoplexes occurred solely by CME (Rejman et al., 2005). In  
42 sharp contrast, Lazebnik *et al.* reported that the specific cationic lipid/siRNA particles they  
43 used were mostly internalized through macropinocytosis (Lazebnik et al., 2016).

44 Each and every endocytic pathway converges at the endo-lysosomal system (Figure 8,  
45 step C). Indeed, lipoplexes that are internalized through CME are finally trapped in the  
46 endosomes. The content next undergoes enzymatic attack in the endo-lysosomes, such that  
47 the NA cargo has little or no access to target. This implies that the lipoplex escape from the  
48 endosomes is essential for efficient transfection. This can be achieved by adding the co-lipid

1 DOPE to cationic lipids and/or using a multivalent cationic lipid (Walsh et al., 2013). On the  
2 other hand, lipoplexes that are internalized through the CvME pathway associate first with the  
3 cell membrane, become trapped into relatively stationary caveolae characterized by the  
4 presence of caveolin, and subsequently are taken up into caveosomes (Durymanov and  
5 Reineke, 2018). Although it was originally hypothesized that lipoplexes internalized through  
6 the caveolae-mediated pathway do not end up in the lysosomes (Rejman et al., 2005), later  
7 studies highlighted that the internalized cargo just goes into the lysosomes (Engel et al., 2011).  
8 In order to induce the endo-lysosomal escape of lipoplexes, the vast majority of scientists have  
9 pointed to the decoration of lipoplexes with peculiar features which can be conveniently  
10 exploited in the acidic environment of the endosome. To this aim, lipoplexes able to undergo  
11  $L_{\alpha}^C$  to  $H_{II}^C$  phase transition when trapped within the endosomal vesicles is by far the most  
12 beaten path (Rehman et al., 2013; Torchilin, 2006). In this regard, transition to non-bilayer  
13 phases is known to induce some thermodynamic instability, which, in practice, means that  
14 fusion of the cationic lipids with the anionic membrane phospholipids takes place (Caracciolo  
15 and Amenitsch, 2012; Koynova et al., 2006). Even more specifically, some phase transitions  
16 occurring at lipoplex level destabilize the vesicle membrane by means of flip-flop transitions  
17 of the outer anionic phospholipids to the inner leaflet, and subsequent ion-pairing with the  
18 cationic lipids that gives rise to the release of intra-vesicular cargo (Xu and Szoka, 1996).  
19 However, it has not been fully elucidated yet whether this process truly consists in a fusion  
20 mechanism, an endosomal membrane destabilization or an endosomal rupture (Jones et al.,  
21 2013; Zuhorn et al., 2007). Recent findings indicated that the endosomal destabilization  
22 process operated by cationic lipids is entropy-driven just as complexation, and the release of  
23 counterions from opposite-charged lipids has been assumed to trigger the disruption of  
24 endosomal vesicles (Avital et al., 2016). Besides, Rehman *et al.* observed that, at the time of  
25 endosomal escape, neither complete endosome rupture nor release of intact lipoplexes into  
26 the cytosol occurred (Rehman et al., 2013). Rather, they observed the formation of multiple  
27 and transient pores studding the endosomal membrane, and through which the genetic cargo  
28 was slowly transferred to the cytosol.

29 Even though endo-lysosomal escape is believed to be the most critical step standing in  
30 the way of efficient NAs delivery, the specific site where NAs elicit their functions deserves  
31 some attention as well (Figure 8, step D). In this regard, whether and once NAs are released  
32 from the endo-lysosomes, while RNAs exploit their function into the cytosol, DNA molecules  
33 have to enter the nucleus. Therefore, the spatio-temporal factors involved in the intracellular  
34 transport of NAs have to be taken into account (Nguyen and Szoka, 2012). As suggested by  
35 others (Cardarelli et al., 2016), intracellular trafficking, endosomal escape and lysosomal  
36 degradation can be viewed as interdependent phenomena, in such a way that they appear as  
37 a single barrier on the route for efficient transfection.

38

### 39 **5. Concluding remarks**

40 Over the last decades, great effort has been devoted to the development of more and  
41 more efficient systems enabling the delivery of NAs into a wide variety of cells. In this context,  
42 lipid-based non-viral vectors have emerged as the most promising delivery systems, such that  
43 few of them have entered clinical trials. Despite early enthusiasm for the use of these vectors,  
44 there is still a long way to go in order to meet the increased expectations. A rational design of  
45 lipoplex formulations is thus required to obtain functional particles with precise and  
46 reproducible physico-chemical features and improved biological activity. In this light, one must  
47 keep in mind each and every factor affecting the performances of lipoplexes. Unfortunately,  
48 there is still no general consensus on the features that a lipidic vector should have to be

1 effective. Rather, different cationic lipids and formulations work better for specific cell types  
2 and applications. Though there have been some examples of real improvements in the design  
3 of lipid delivery vectors, results escaped general consensus because somewhat inconsistent  
4 and patchy. It turns out that improvement in the design of transfectants is perceived as  
5 cumbersome and frustrating. Our belief is that constant improvements in lipofection will be  
6 made possible through more comprehensive mechanistic investigations and SAR studies.  
7 This is the main challenge that chemists, materials scientists, bioengineers and  
8 pharmacologists shall strive for.

9

#### 10 **Acknowledgements**

11 We wish to thank Politecnico di Milano for financial support.

12



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